

Manuscript version: Author's Accepted Manuscript

The version presented in WRAP is the author's accepted manuscript and may differ from the published version or Version of Record.

Persistent WRAP URL:

<http://wrap.warwick.ac.uk/102724>

How to cite:

Please refer to published version for the most recent bibliographic citation information. If a published version is known of, the repository item page linked to above, will contain details on accessing it.

Copyright and reuse:

The Warwick Research Archive Portal (WRAP) makes this work by researchers of the University of Warwick available open access under the following conditions.

Copyright © and all moral rights to the version of the paper presented here belong to the individual author(s) and/or other copyright owners. To the extent reasonable and practicable the material made available in WRAP has been checked for eligibility before being made available.

Copies of full items can be used for personal research or study, educational, or not-for-profit purposes without prior permission or charge. Provided that the authors, title and full bibliographic details are credited, a hyperlink and/or URL is given for the original metadata page and the content is not changed in any way.

Publisher's statement:

Please refer to the repository item page, publisher's statement section, for further information.

For more information, please contact the WRAP Team at: wrap@warwick.ac.uk.

Title:

Haptic foot pedal: influence of shoe type, age, and gender on subjective pulse perception

Authors:

Geitner, Claudia¹; Birrell, Stewart^{1*}; Krehl, Claudia² and Jennings, Paul¹

¹Warwick Manufacturing Group (WMG). University of Warwick, International Digital Laboratory, Coventry, CV4 7AL, UK.

²HMI Research Team. Jaguar Land Rover. University of Warwick, International Digital Laboratory, Coventry, CV4 7AL, UK.

*corresponding author

50 words abstract:

This study investigates the influence of shoe type (sneakers and safety boots), age and gender on the perception of haptic pulse feedback provided by a prototype accelerator pedal in a running stationary vehicle. Drivers within three age groups (“≤ 39”, “40-59” and “≥ 60”) took part.

Biographies:

Claudia Geitner:

Claudia Geitner graduated in Media-Computer-Science at the Dresden University of Technology (Germany). The major subject and major research interest was Human-Computer Interaction. She then proceeded to work in the field of Human Factors in the areas of web design and power plant design. Claudia is currently an Engineering Doctorate candidate at the University of Warwick (UK) researching into how drivers interact with new in-vehicle technology and effects of that interaction on the driving behaviour.

Stewart Birrell:

Stewart A. Birrell has a BSc (Hons) degree in Sport Science from the University of Hertfordshire and a PhD in Ergonomics from Loughborough University. His primary research interests concern how humans interact with their surroundings and subsequent effect on task outcome and performance, which has been developed through working within a variety of different domains such as sport, military and transport. Stewart has recent experience in the design and evaluation of in-vehicle systems, where currently he works as an Assistant Professor at University of Warwick investigating human factors aspects of low carbon transport. Stewart has numerous scientific papers published in the field of Human Factors.

Claudia Krehl:

Claudia Krehl obtained her PhD 2014 at the University of Nottingham, investigating how Human Computer Interaction for Mobile Devices can be improved in multitasking situations with multimodal and context aware interface designs. Currently, Claudia works as Senior Human Factors Engineer at Jaguar Land Rover.

Paul Jennings:

Professor Paul Jennings is the lead academic for the '3xD Simulator for Intelligent Vehicles, the world's first immersive, simulated environment for smart and connected vehicles. He is Deputy Chief Technology Officer of the University of Warwick's centre High Value Manufacturing Catapult, and has worked for over 25 years on collaborative automotive research, leading projects funded by the Engineering and Physical Sciences Research Council, Innovate UK and the EU, valued at over £20m. He pioneered the use of interactive sound evaluation in the automotive industry through a vehicle simulator now exploited globally by Bruel and Kjaer.

Haptic foot pedal: influence of shoe type, age, and gender on subjective pulse perception

Short title: Factors affecting haptic pulse perception on a foot pedal.

Abstract: This study investigates the influence of shoe type (sneakers and safety boots), age and gender on the perception of haptic pulse feedback provided by a prototype accelerator pedal in a running stationary vehicle. Drivers within three age groups (" ≤ 39 ", "40-59" and " ≥ 60 ") took part.

1 **Objective:** This study investigates the influence of shoe type (sneakers and safety boots), age and gender on the
2 perception of haptic pulse feedback provided by a prototype accelerator pedal in a running stationary vehicle.

3 **Background:** Haptic feedback can be a less distracting alternative to traditionally visual and auditory in-vehicle
4 feedback. However, to be effective the device delivering the haptic feedback needs to be in contact with the person.
5 Factors, such as shoe type, vary naturally over the season and could render feedback that is perceived well in one
6 situation, unnoticeable in another. In this study, we evaluate factors that can influence the subjective perception of
7 haptic feedback in a stationary but running car: shoe type, age, and gender.

8 **Method:** Thirty-six drivers within three age groups (" ≤ 39 ", "40-59" and " ≥ 60 ") took part. For each haptic feedback,
9 participants rated intensity, urgency and comfort via a questionnaire.

10 **Results:** The perception of the haptic feedback is significantly influenced by the interaction between the pulse's
11 duration and force amplitude, and by the participant's age and gender, but not shoe type.

12 **Conclusion:** The results indicate that it is important to consider different age groups and gender in the evaluation
13 of haptic feedback. Future research might also look into approaches to adapt haptic feedback to the individual
14 driver's preferences.

15 **Application:** Findings from this study can be applied to the design of an accelerator pedal in a car, e.g. for a non-
16 visual in-vehicle warning, but also to plan user studies with a haptic pedal in general.

17 **Keywords:** tactile interaction, haptic perception, driver assistance system

18 INTRODUCTION

19 Haptic feedback can be an alternative to visual and auditory in-vehicle feedback, interfering less with
20 the primarily visual-cognitive task of driving. Previous studies demonstrated that haptic feedback, such
21 as vibration or counterforce, can reduce the driver's workload when presented while the driver interacts
22 with non-driving relevant information, e.g. the in-vehicle infotainment system (Lee, Hoffman, and Hayes,
23 2004; Brown, 2005; Birrell, Young, and Weldon, 2013). Adell, Várhelyi, and Hjälmdahl (2008) even
24 identified a haptic pedal with counterforce as a preferred solution for warnings when speeding,
25 compared to an acoustic and visual warning. To be effective, users need to perceive the haptic feedback
26 as clearly noticeable, but still comfortable (Abbink, 2006). In this study, we evaluate how factors that
27 vary naturally within users influence the subjective perception of haptic feedback: shoe type, age, and
28 gender.

29 Drivers perceive haptic feedback from a pedal via their shoe. A driver's footwear can vary notably over
30 the year. So far, the shoe type was rarely subject of evaluations. Abbink and Van der Helm (2004) and
31 Ichinose, Gomikawa, and Suzuki (2013) evaluated the just noticeable perception of haptic pulses,
32 varied in force amplitude and frequency, on the foot via the shoe. Participants wearing shoes with stiff

33 soles needed comparable greater force amplitudes to perceive the pulse. The difference in perception
34 between the shoe types appears to decrease as the pulses become more noticeable. More research is
35 needed to understand if the influence of shoe type reduces as pulse noticeability increases, and that if
36 these increase in either amplitude, force or duration mean that the feedback is still perceived as
37 comfortable by the user.

38 Shoe types might influence the perception of haptic feedback particularly in older drivers. Whereas
39 previous driving related studies related to haptic pedal interfaces included mainly young participants
40 (De Rosario et al., 2010; Ichinose et al., 2013; Abbink and Van der Helm, 2004), other research has
41 shown that physical perception of haptic feedback appears to decline with age (Inglis, Kennedy, Wells,
42 and Chua, 2002; Brown, 2005; Perry, 2006; Shaffer and Harrison, 2007). Perry (2006) found that older
43 participants were less sensitive to vibrations of greater than 100 Hz. Early research by Verrillo (1982)
44 came to a similar conclusion, comparing the perception of 25 and 250 Hz on the hand. The results
45 emphasize the need to consider older people when evaluating the perception of in-vehicle haptic
46 feedback to ensure its noticeability.

47 Feedback presented to the driver should be balanced between being easy to notice, but not startling.
48 Startling feedback can increase the drivers' reaction time (Biondi, Rossi, Gastaldi, and Mulatti, 2014).
49 This balance is not easy to achieve. For example, literature suggests differences in haptic perception,
50 specifically that of comfort, between gender. Females seem to be more sensitive to pressure on the
51 skin (Hale and Stanney, 2004) and to vibration (Hennig and Sterzing, 2009). However, literature varies,
52 Hennig and Sterzing (2009) did not find a gender-related difference in the perception of touch and
53 Schlee (2010) did not discover a gender-related perceptual threshold difference in vibration. An
54 explanation could be that sensitivity decreases with age, but more so for males compared to females
55 (Halonen, 1986; Hiltz, Axelrod, Hermann, Haertl, Duetsch, and Neundörfer, 1998). This study evaluated
56 gender as a potential influence on the perception of intensity and comfort of a haptic feedback.

57 This study assessed a single haptic pulse that can be envisioned as a bump, comparable to a tap with
58 the finger. In this study the haptic pulse was modified by force amplitude (intensity of the touch) and
59 duration. Preliminary findings were presented in Geitner, Birrell, Skrypchuk, Krehl, and Jennings (2015),
60 with this current paper extending the analysis and recommendations to include all pulse settings
61 evaluated as well as further considering the effects of age and gender.

62 To the authors' knowledge, there is no study evaluating the combined effects of shoe type (sneakers
 63 and safety boots), age, and gender on the subjective perception of haptic pulse feedback from a pedal
 64 in a car. They are evaluated together in this study. As literature suggests, all three variables could
 65 influence haptic perception.

66 MATERIALS AND METHOD

67 This study assessed the influence of shoe type, age and gender on the subjective perception of haptic
 68 pulses. It is hypothesized that:

- 69 • Shoes with a thicker and stiffer sole influence the perception of haptic pulses negatively, but only
 70 for just noticeable pulse feedback
- 71 • Age has a negative influence on the perception of haptic pulses.
- 72 • Females are expected to perceive the intensity of haptic feedback stronger than males.

73 Participants

74 Thirty-six people took part and were included in the analysis of the data. Normal haptic perception and
 75 no known illness affecting haptic perception, such as diabetes (Travieso and Lederman, 2007), were
 76 prerequisites for participation in this study.

77 To test the hypothesis, participants were distributed across three age groups and both genders, similar
 78 to that used by Mehler, Reimer, and Coughlin (2011) to evaluate physiological workload measures.

79 **Table 1.** Overview of the participants in the study.

	Age "≤ 39" years		Age "40 – 59" years		Age "≥ 60" years	
	Male	Female	Male	Female	Male	Female
Number of participants	6	5	8	5	7	5
All participants in an age group	11		13		12	

80 The University of Warwick's Biomedical and Scientific Research Ethics Committee approved the study
 81 (REGO-2014-1312).

82 **Apparatus**

83 *Equipment.* The study was conducted in a stationary but running Range Rover vehicle with an
84 implemented proprietary haptic pedal prototype (Figure 1). According to the hypothesis, two shoe types
85 were evaluated: shoes with a thick and stiff sole (safety boots) and shoes with a thin and flexible sole
86 (sneakers). The shoes were provided to the participant to avoid unwanted variations. Beforehand, a set
87 of shoe sizes (sizes 5 to 10) had been estimated that would cover 95% of the population. The
88 participants wore their own socks in the shoes. Both shoe types were comparable in weight. Soles were
89 approximately 8 millimeter (mm) for the sneakers and 14 mm for the safety boots.

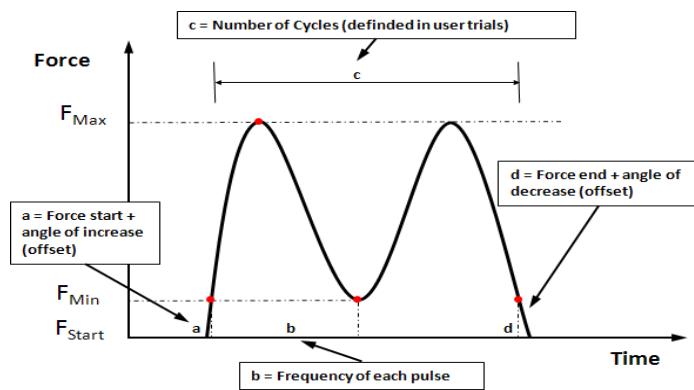


90
91 **Figure 1.** Study equipment.

92 *Selection of pulses.* Pulse settings in this study were presented by force amplitude in Newton (N), and
93 duration in milliseconds (ms). One pulse can be considered as a single vibration. A pulse's duration can
94 then be expressed as frequency. The term duration is used throughout this study. Frequency (in Hertz
95 (Hz)) is mentioned additionally for comparison with related literature that applied frequency in Hz. The
96 pulses were presented as sine-shaped waveform (Figure 2). Activation of the feedback required the
97 pedal to be depressed. During a pulse, the pedal moved upwards in the set parameters, adjusted by a
98 software.

99 The pulse settings were selected in a range from just noticeable to clearly noticeable, constrained by
100 the prototype haptic pedal implemented in the car. The force amplitude was adjustable from 6-21 N and
101 the duration from 2 s to 16 ms (0.5 - 62.5 Hz). Following findings from Abbink and Van der Helm (2004)
102 and Ichinose et al. (2013), 9 N / 1 s was selected as just noticeable feedback and 7 N / 1 s as just below
103 the noticeable feedback for shoes with thin and flexible soles (1 s = 1 Hz for a single pulse). The highest
104 amplitude was 18 N, selected after a pilot in which pulses with greater amplitudes were perceived as

105 either uncomfortable or too strong. The durations 67, 33, and 20 ms were selected to cover the
 106 spectrum available by the haptic pedal prototype. Table 2 lists all pulse settings selected for this study.



107

108 **Figure 2.** Pulse in sine-shaped waveform.

109 **Table 2.** Sixteen pulses were employed in this study; Top - Force amplitudes in Newton (N), Middle - Duration of the pulse
 110 expressed as frequency in Hertz (Hz), and Bottom - Duration of the pulse in milliseconds (ms).

7 N	9 N	14 N	18 N	7 N	9 N	14 N	18 N	7 N	9 N	14 N	18 N	7 N	9 N	14 N	18 N
1 Hz	1 Hz	1 Hz	1 Hz	15 Hz	15 Hz	15 Hz	15 Hz	30 Hz	30 Hz	30 Hz	30 Hz	50 Hz	50 Hz	50 Hz	50 Hz
1000 ms	1000 ms	1000 ms	1000 ms	67 ms	67 ms	67 ms	67 ms	33 ms	33 ms	33 ms	33 ms	20 ms	20 ms	20 ms	20 ms

111 *Experimental environment.* Literature and pilot studies indicated that haptic perception varies over the
 112 sole of the foot (Inglis et al., 2002; Kennedy and Inglis, 2002). The heel and toe region seem to be more
 113 sensitive than ball and arch. Also, joints, tendons and muscles are activated when the leg moves (e.g.
 114 depressing the pedal) and contribute to the haptic perception (Hale and Stanney, 2004). They could
 115 result in different perception of a haptic pulse presented on the foot dependent on seating position and
 116 movement of the leg. Those considerations led to the following experimental settings to control for
 117 extraneous variables:

- 118 • *Position of the seat:* The participants were required to adjust the seat to a position suitable for
 119 driving, where they could comfortably reach the pedals and steering wheel.
- 120 • *Position of the foot on the pedal:* To ensure a comparable equal contact between the foot and pedal,
 121 participants were instructed to use their whole foot on the pedal. Additionally, they were instructed
 122 to keep the heel on the ground, making it easier to hold the pedal in a stable position. Some
 123 participants who had difficulty reaching the pedal just kept their whole foot on the pedal as priority.

- 124 • *Pedal angle*: To ensure a consistent pedal angle (and subsequent force which needed to be
125 applied) haptic feedback commenced when the vehicle's RPM (revolutions per minute of the
126 engine) was stable at between 1,500 and 2,000 RPM. Using this RPM setting helped ensure the
127 haptic feedback was presented when the pedal travel was minimal.
- 128 • *Vibrations of the car itself*: The study was conducted in a static but running car to increase realism
129 (e.g. with vibration of the engine) and applicability of results. The background vibration was kept
130 stable through the applied controlled range of RPM.
- 131 • *Temperature in the cabin*: Temperature in the cabin was controlled at a comfortable range for the
132 participant.

133 Questionnaire for perception of the haptic feedback

134 The participants rated each haptic pulse with three questions concerning intensity, comfort and urgency
135 (how much a pulse motivates reaction) (Table 3). Abbink's (2006) suggestion, to balance comfort and
136 clear perception of haptic feedback, resulted in two questions about comfort and intensity of perception
137 in this study. Uncomfortable feedback carries the risk to startle the driver, which would increase the
138 reaction time, and is adverse for a warning related to safe driving. Employing urgency as a dimension
139 can help in the development of an incremental warning including warnings that trigger a faster reaction
140 from the driver. Therefore, a question addressing urgency was added. Comfort and urgency were rated
141 on a seven-point rating scale similar to Brown (2005). Intensity was rated on a five-point rating scale as
142 found in (Kaaresoja and Linjama, 2005).

143 **Table 3.** Subjective ratings for each pulse.

(1) Was the feedback perceived?

1	2	3	4	5
Not detected	Weak	Moderate	Strong	Too strong

(2) How comfortable was the feedback?

1	2	3	4	5	6	7
Not comfortable						Very comfortable

(3) How urgent did the feedback feel? (if participants feel they should react to the feedback)

1	2	3	4	5	6	7
Not urgent						Very urgent

144 **Procedure**

145 The participants were introduced to the study, signed an institutional consent form, and adjusted the
146 seat to a position they would take for driving and started the car. Before the start of the study they
147 familiarized themselves with the haptic pedal. They depressed the pedal and when a stable position of
148 the pedal was found (e.g., between 1,500 and 2,000 RPM), the experimenter presented two varying
149 example pulses (not part of the set, e.g., 10 N / 50 ms). The participants practiced rating their perception
150 by answering three questions after the perception of each pulse (Table 3).

151 The participants experienced either sneakers or safety boots first, in a counterbalanced order across
152 age and gender. The set of sixteen pulses (Table 2) was randomized six times. Three of those
153 randomized sets were presented to the participants in the first shoe condition and the other three in the
154 second shoe condition. The experimenter initiated a pulse when the participant kept the foot in a stable
155 position on the pedal, between 1,500 and 2,000 RPM. After perceiving one pulse, the participant rated
156 this pulse in (1) intensity, (2) comfort, and (3) urgency (Table 3), always in that order. For an efficient
157 and consistent procedure during the study, participants were advised to keep the foot on the pedal and
158 the pedal depressed during one set of sixteen pulses. Abbink and Van der Helm (2004) mentioned that
159 participants applied varying rating strategies for the perception of the pulses. This variation was one of
160 the reasons which led to a repeated measure design in this study. The study lasted approximately one
161 hour per participant.

162 **Data Analysis**

163 The data analysis was conducted in R (R Core Team, 2014). Pulses that were not detected by the
164 participants were rated as 1 in intensity ("Not detected"), and no urgency and comfort rating were
165 recorded. The ratings for intensity, and comfort were interpreted with parametric statistics. Each
166 participant perceived and rated each pulse six times (three times in each shoe condition), each time for
167 intensity, comfort, and urgency. The three repeated ratings for (each) intensity, urgency and comfort for
168 a pulse in one shoe condition were aggregated into a mean rating, to reach a comparably balanced
169 rating with the participant adjusting to the rating scales during the repeated representation of pulses.

170 Mean comfort ratings were widely distributed with a standard deviation (SD) ranging from 1.35 to 1.6
171 (on a 7-point rating scale). It might have resulted from different rating strategies. Some participants took
172 the middle of the scale as baseline, whereas others rated comfort high unless they felt uncomfortable
173 with their foot. To take the individual strategies into account, a new comfort classification was generated
174 referred to as “balanced comfort” (BC). Balanced comfort was calculated by the z-score formula. By
175 applying the formula the individual mean rating for a participant are considered and the comfort rating
176 could be compared along its standard deviation to that mean. First, the mean comfort rating over all
177 pulses (p) and shoe conditions (s) was calculated for each participant. Then this mean comfort rating
178 over all pulses (μ) for a participant was subtracted from the specific participant’s comfort rating for the
179 current pulse ($c_{s,p}$). Last, the subtraction was divided by the standard deviation of the participant’s
180 comfort ratings (σ). The further analysis was based on these balanced comfort ratings. This balancing
181 technique was only employed for the comfort ratings as these ratings had the highest variance and
182 visually different rating patterns.

$$183 \quad BC = (c_{s,p} - \mu) / \sigma \mid 1 \leq s \leq 6, 1 \leq p \leq 16$$

184 In the descriptive presentation, intensity and urgency ratings appeared to follow a similar pattern.
185 Therefore, a two tailed Pearson Product Correlation test was conducted. The result suggests a strong
186 positive correlation between intensity and urgency ratings, $r(2904) = .81, p < .001$. Due to the strong
187 correlation of the urgency and intensity ratings, the analysis for the urgency ratings is not presented in
188 more detail.

189 An ANOVA analysis was conducted to evaluate effects of shoe, age and gender on the ratings of
190 intensity of the haptic pulses, each with a critical value of $p < 0.05$. The ANOVA included an error
191 calculation for the within subject variables (shoe, force amplitude and duration). The analysis considers
192 main effects of age, gender, and shoe type only. The sample size would be too small to return a suitable
193 power for analyzing potential effects between age groups, if we split by gender. Comfort ratings were
194 analyzed with t-tests, due to the reduced number of comfort ratings when pulses were not perceived.

195

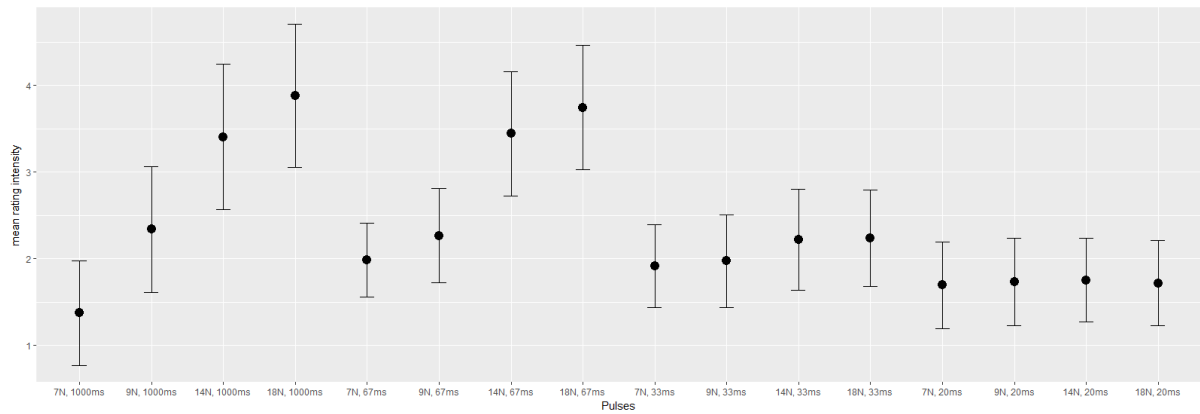
RESULTS

196 The data set was tested for homogeneity of variance with the Levene test and met that criterion. Then
197 an omnibus mixed model ANOVA analysis was conducted to evaluate the intensity ratings. The model
198 included perception as an independent variable and age, gender, shoe, duration and force amplitude
199 as dependent variables. The model included an error correction for the within subject variables shoe,
200 duration, and force amplitude. Its results suggested interaction effects of duration, force amplitude,
201 gender and age on the perception of the pulses. The influence of gender ($F(1,30) = 5.05, p = 0.03$),
202 force amplitude ($F(3,90) = 496.66, p < .001$) and duration ($F(3,90) = 253.09, p < .001$) is significant
203 overall. The effects of the between subject variables age and gender were analyzed in detail with the
204 Tukey HSD.

205 **Experience of the Pulses Overall**

206 The variability of the ratings over all the pulses were as follows: standard deviations (SDs) between
207 0.42-0.82 for intensity, SDs between 0.98-1.45 for urgency and SDs between 0.53-1.37 for balanced
208 comfort. Over all pulse settings, force amplitude and duration of the pulses were rated significantly
209 different, indicating the participants perceived them as different ($F(9,270) = 206.36, p < .001$). Duration
210 seemed to be the main influence on perception of the haptic pulse feedback, giving it a characteristic.

211 The data examined across each combination of force amplitude and varying durations can be described
212 by different perceptual patterns, grouped either by duration (Figure 3) or by force amplitude. The
213 intensity rating for a pulse of a certain duration increased with larger force amplitude. Intensity ratings
214 for durations of 1000 ms rose steeply with higher force amplitudes, from just detectable in combination
215 with the lowest force amplitude (7 N) to strong in combination with 18 N. Similarly, intensity ratings for
216 67 ms pulses increased with stronger force amplitudes to a mean intensity rating between moderate
217 and strong (rating 3-4). The intensity ratings for pulses with a duration of 33 ms increased only slightly
218 with higher force amplitude. Pulses of the shortest duration of 20 ms were an exception from that
219 pattern. They were rated hard to perceive independent from the combined force amplitude. In addition,
220 over all pulses, 7 N was rated as just perceivable or weak in this study. Pulses with a force amplitude
221 of 7 N also included the highest percentage of not perceived pulses (rated as "not detected").



222

223

Figure 3. Mean ratings for intensity calculated over all participants and both shoe conditions (the rating scale in Table 3, question (1)). The mean intensity rating is presented for all sixteen pulses sorted by duration.

224

225

Ratings for balanced comfort showed an inverse pattern to intensity ratings, increasing from pulses rated high in intensity to being highest for pulses rated as weak in intensity. Pulses rated as “too strong” in intensity tended to receive a negative comfort rating (Table 3). Given the rating scale selected, an optimal rating for pulse intensity could be considered between 3 (moderate) and 4 (strong). A rating of 5 states “too strong” on the rating scale indicating a negative bias, a potential to startle the driver. The negative bias of an intensity rating of 5 is supported by participant’s negative comfort rating.

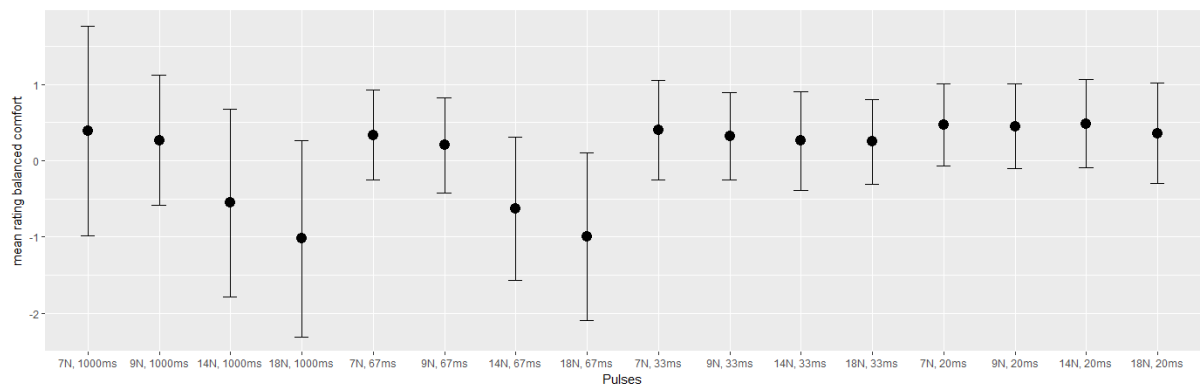
226

227

228

229

230



231

232

Figure 4. Mean ratings for balanced comfort for all pulses (not comfortable – negative, neutral – 0, comfortable – positive).

233 Effect of Shoe Type on Perception

234

In contrast to the previous study by Abbink and Van der Helm (2004), intensity ratings in this study did not differ significantly between the two shoe conditions, $F(1,30) = 0.28$, $p = 0.6$. There were no significant interactions between shoe type and the other variables of the ANOVA model. Potential reasons, such as the more realistic study design, are described in the Section “Discussion and Conclusion”. Due to the non-significant result, no post-hoc analysis was conducted.

235

236

237

238

239 **Effect of Age on Perception**

240 In the overall repeated measure ANOVA analysis age itself appeared not to have a significant effect
 241 alone on the intensity of the pulses ($F(1,30) = 0.04, p = 0.95$). However, the omnibus ANOVA analysis
 242 showed significant interaction effects between age and force amplitude ($F(6,90) = 2.39, p = 0.03$);
 243 between age and duration, ($F(6,90) = 2.45, p = 0.03$); and between age, duration, and gender,
 244 ($F(6,90) = 2.77, p = 0.01$). A post-hoc analysis with Tukey HSD revealed that the youngest age group
 245 (≤ 39) and the oldest age group (≥ 60) rated the short duration pulses of 20 ms ($p = 0.03$) and 33 ms
 246 ($p = 0.006$) significantly different in intensity.

247 **Table 4.** Overview of mean ratings for intensity and balanced comfort compared across age groups (the percentage of missed
 248 pulses was calculated with respect to the number of ratings in the specific age group, because the age groups are not equally
 249 distributed).

		Pulse feedback settings: Force Amplitude in Newton (N) and duration in millisecond (ms)															
		7N	9N	14N	18N	7N	9N	14N	18N	7N	9N	14N	18N	7N	9N	14N	18N
		1000 ms	1000 ms	1000 ms	1000 ms	67 ms	67 ms	67 ms	67 ms	33 ms	33 ms	33 ms	33 ms	20 ms	20 ms	20 ms	20 ms
age group " ≤ 39 "	Mean rating for intensity	1.46	2.36	3.24	3.91	1.95	2.20	3.35	3.67	2.03	2.09	2.3	2.38	1.73	1.83	1.74	1.79
	Percentage of missed pulses	57.6%	4.5%	3%	0	13.6%	4.5%	0	0	7.6%	7.6%	6.1%	0	31.8%	22.7%	27.3%	21.2%
	Mean rating bal. comfort	0.68	0.18	-0.81	-1.1	0.35	0.29	-0.67	-1.05	0.5	0.38	0.29	0.32	0.4	0.43	0.43	0.37
age group " $40-59$ "	Mean rating for intensity	1.37	2.32	3.36	3.71	2.01	2.31	3.4	3.67	1.91	1.99	2.19	2.15	1.77	1.76	1.82	1.77
	Percentage of missed pulses	70.5%	5.1%	1.3%	1.3%	5.1%	1.3%	0	0	15.4%	16.7%	7.7%	9%	24.4%	27%	21.8%	27%
	Mean rating bal. comfort	0.02	0.35	-0.41	-0.95	0.35	0.1	-0.57	-0.92	0.29	0.27	0.26	0.16	0.4	0.46	0.45	0.3
age group " ≥ 60 "	Mean rating for intensity	1.27	2.33	3.61	4.03	1.98	2.28	3.58	3.9	1.81	1.85	2.17	2.19	1.58	1.61	1.68	1.6
	Percentage of missed pulses	77.8%	15.3%	0	0	11%	4.2%	0	0	25%	20.8%	5.6%	5.6%	41.7%	38.9%	33%	41.7%
	Mean rating bal. comfort	0.41	0.27	-0.48	-0.99	0.31	0.23	-0.67	-1.03	0.42	0.31	0.23	0.28	0.64	0.45	0.59	0.43

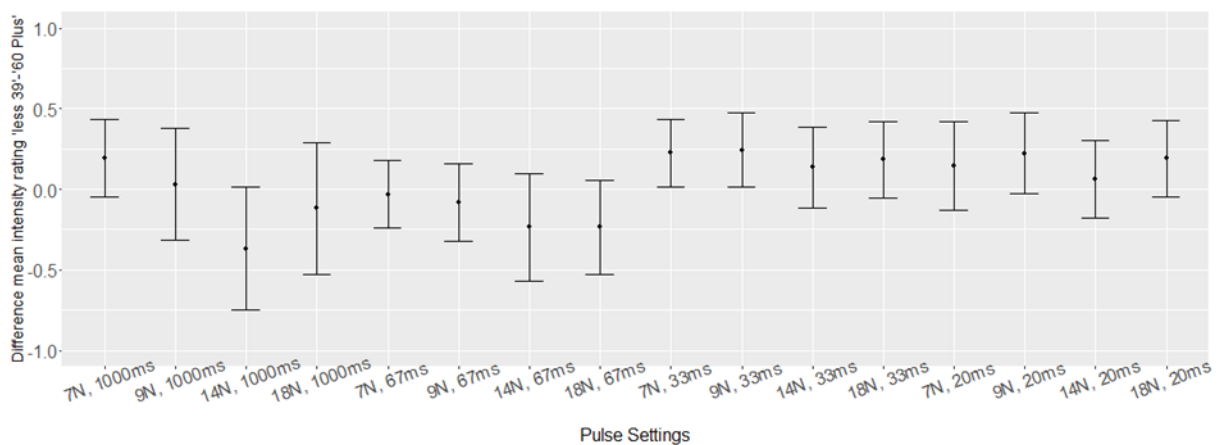
Coding for Table 4

Mean intensity rating:	dark grey: ≤ 2 (hardly noticeable)	medium grey: >2 & ≤ 3 (weak)	white: >3 & ≤ 4 (moderate)	light grey: >4 (strong)
Percentage of missed pulses:	dark grey: $>20\%$	medium grey: >5 & $\leq 20\%$	white: 0	light grey: $\leq 5\%$
Mean rating bal. comfort:	dark grey: ≤ -1	medium grey: >-1 & ≤ 0	white: >0 or 0	

250 Table 4 provides an overview of the participants' intensity and comfort ratings, and percentage of
 251 missed pulses for each evaluated force amplitude and duration combination for all three age groups.
 252 The shades of grey mark levels of intensity, percentage of missed pulses, and levels of balanced
 253 comfort. Pulses with longer durations were rated in average higher in intensity and a smaller number of
 254 pulses was missed, in all age groups (lighter shade). Over all pulses, the oldest age group missed a

255 higher percentage of pulses compared to the other age groups (darker shade). Pulses that were rated
 256 high in intensity (18 N / 1000 ms, 14 N / 67 ms and 18 N / 67 ms) tended to be rated as less comfortable
 257 (darker shade).

258 Differences in the mean intensity ratings for each pulse between the age groups were calculated in
 259 order to further evaluate the influence of age on pulse intensity. Figure 5 shows the calculated difference
 260 between the age groups “≤ 39” and “≥ 60” as a black dot for each pulse and the 95% confidence
 261 intervals as a black bar. A positive difference in the short duration pulses indicated higher intensity
 262 ratings by the youngest age group. As the range of the confidence intervals was mostly positive for the
 263 short duration pulses (33 ms and 20 ms), this supports the assumption that shorter duration pulses are
 264 easier to perceive for the younger age group compared to the oldest age group.



265
 266 **Figure 5.** Difference in mean ratings for intensity (youngest age group “≤ 39” minus oldest age group “≥ 60”).

267 **Effect of Gender on Perception**

268 Table 5 provides an overview of the participants’ intensity and comfort ratings for each evaluated force
 269 amplitude and duration combination across gender. The shades of grey mark levels of perceived
 270 intensity, percentage of missed pulses, and ratings for comfort. Overall, female and male participants
 271 rated the intensity of the haptic pulses significantly different ($F(1,18) = 5.05, p = 0.03$). Females gave a
 272 higher intensity rating and missed less pulses compared to males in all pulse settings (Table 5).
 273 However, females tended to rate a pulse that was rated high in intensity on average as less comfortable
 274 compared to males, specifically durations of 1000 ms combined with the force amplitudes of 14 and
 275 18 N. Females ($M = 0.51$) perceived shorted duration pulses as significantly more comfortable
 276 compared to male participants ($M = 0.38$), $t(171.62) = 2.0, p = 0.04$. Females ($M = -0.59$) also rated

277 longest duration pulses as significantly more negative compared to males ($M = -0.09$), $t(232.7) = -3.64$,
 278 $p = 0.0003$.

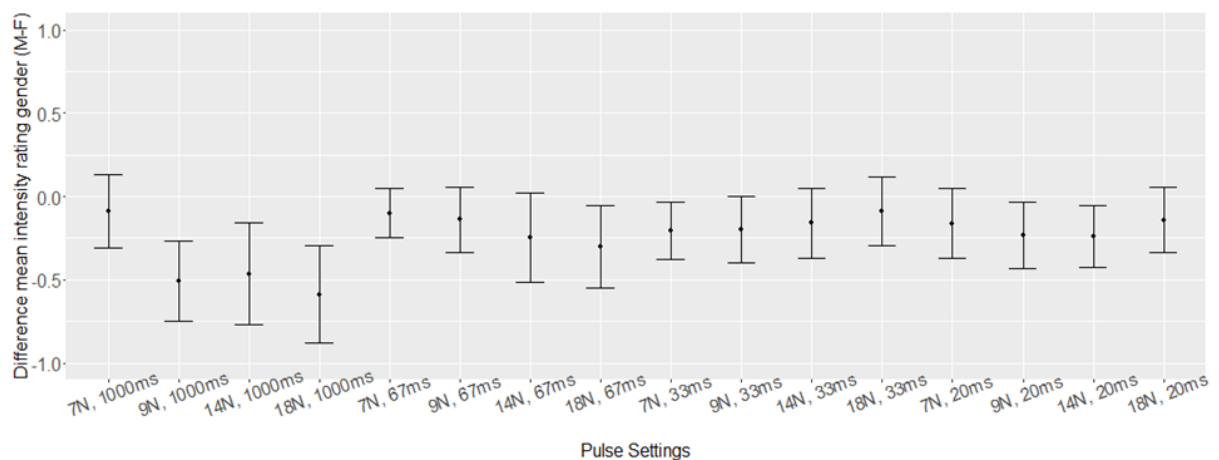
279 **Table 5.** Overview of mean ratings for intensity and balanced comfort compared across genders (the percentage of missed
 280 pulses is calculated with respect to the number of ratings in the specific gender, because gender is not equally distributed).

		Pulse feedback settings: Force Amplitude in Newton (N) and duration in millisecond (ms)															
		7N 1000 ms	9N 1000 ms	14N 1000 ms	18N 1000 ms	7N 67 ms	9N 67 ms	14N 67 ms	18N 67 ms	7N 33 ms	9N 33 ms	14N 33 ms	18N 33 ms	7N 20 ms	9N 20 ms	14N 20 ms	18N 20 ms
female	Mean rating intensity	1.42	2.63	3.68	4.22	2.04	2.34	3.59	3.92	2.03	2.09	2.31	2.29	1.79	1.87	1.89	1.8
	Percentage of missed pulses	64.3%	3.3%	3.3%	1.1%	5.5%	3.3%	0	0	5.5%	5.5%	3.3%	1.1%	24.4%	18.8%	14.4%	21.1%
	Mean rating bal. comfort	0.2	0.11	-0.98	-1.5	0.46	0.28	-0.75	-1.04	0.5	0.48	0.43	0.37	0.46	0.47	0.55	0.55
male	Mean rating intensity	1.33	2.12	3.21	3.63	1.94	2.21	3.34	3.61	1.83	1.89	2.15	2.2	1.63	1.63	1.65	1.66
	Percentage of missed pulses	72.2%	11.9%	0	0	12.6%	3.1%	0	0	23.8%	22.2%	8.7%	7.9%	38.1%	37.3%	36.5%	36.5%
	Mean rating bal. comfort	0.57	0.39	-0.26	-0.68	0.24	0.14	-0.54	-0.96	0.32	0.18	0.13	0.16	0.47	0.43	0.42	0.19

Coding for Table 5

Mean intensity rating:	dark grey: ≤ 2 (hardly noticeable)	medium grey: > 2 & ≤ 3 (weak)	white: > 3 & ≤ 4 (moderate)	light grey: > 4 (strong)
Percentage of missed pulses:	dark grey: $> 20\%$	medium grey: > 5 & $\leq 20\%$	white: 0	light grey: $\leq 5\%$
Mean rating bal. comfort:	dark grey: ≤ -1	medium grey: > -1 & ≤ 0	white: > 0 or 0	

281
 282 A comparison of the difference in the mean intensity ratings between males and females (mean intensity
 283 rating male minus mean intensity rating female) also suggests a tendency for females to rate pulses
 284 higher in intensity compared to males. The 95% confidence interval for the calculated difference is
 285 mostly negative meaning females rated haptic pulses on average higher than the males (Figure 6).



286
 287 **Figure 6.** Difference in mean ratings for intensity (Males (M) minus Females (F)).

288 The difference between male and female ratings remains when the ratings were divided by age group.
289 For the shortest duration it appeared males in the oldest age group rated intensity on average lower
290 compared to females in this age group and participants of other age groups.

291 **DISCUSSION AND CONCLUSION**

292 A mixed model ANOVA analysis conducted over all variables indicates interaction effects between
293 gender, force amplitude, duration and age on the perception of haptic pulses. In contrast to the
294 hypothesis and previous research by Abbink and Van der Helm (2004) shoe type did not have a
295 significant effect on the perception of haptic pulses in this study. The differences in results are possibly
296 due to differences in the design of the studies. In the present study, there was no counter pressure
297 imposed on the foot which could have decreased the perceived intensity. Also, the more realistic design
298 utilizing a stationary running car added a constant slight vibration. Those factors could have reduced
299 the perception of the just noticeable pulses and therewith eliminated slight differences in shoe types.
300 Other findings from this study are in accordance with previous findings from Abbink and Van der Helm
301 (2004): pulses were perceived more often with a higher force amplitude, except for the shortest duration
302 of 20 ms, and an increasing frequency made lower force amplitudes more perceptible, except for the
303 lowest force amplitude of 7 N.

304 As hypothesized, age seems to affect the perception of haptic pulses, but only in combination with
305 duration. The oldest age group rated the two shortest durations (20 and 33 ms) in average lower in
306 intensity than the two other age groups. Supporting this result, Verillo (1982) has reported a decline of
307 haptic perception with age previously. He found that the sensitivity for vibrations over 25 Hz declined in
308 older participants compared to younger.

309 Overall, gender had a significant effect on the perceived intensity and comfort of the haptic pulses. As
310 hypothesized, females gave a higher mean rating for intensity for all pulses. This finding is supported
311 by Hale and Stanney (2004) who found a higher sensitivity of females in haptic perception of pressure
312 on the skin. Neely, Burström and Johansson (2001) also found females rated intensity and perceived
313 discomfort higher compared to males for vibration on the arm.

314 **Recommendations from the study**

315 Summarizing, the following recommendations are derived from the study's results:

316 ***Duration (frequency) was the main parameter that influenced haptic pulse perception, and gave***
317 ***it a specific characteristic.*** Similarly, MacLean and Enriquez (2003) found frequency as a major
318 influence to perception of haptic icons, compared to amplitude or waveform. Some participants
319 described short duration pulses as a “knock” (similarly found by Brewster and Brown (2004)) and long
320 duration pulses as a “bump”.

321 • ***Durations shorter than 33 ms (in this study it was 20 ms) are not recommended, as they were***
322 ***rated weak in intensity and pulses were missed, independent from the applied force***
323 ***amplitude.*** In their experiment about haptic perception of vibration on the finger, Kaaresojya and
324 Linjama (2005) found pulses of 12.5 ms as not perceivable and those of 25 ms duration hard to
325 perceive. The results match those found herein, and strengthen recommendations to apply
326 durations longer than 20 ms.

327 • ***The duration of 67 ms (15 Hz) is recommended considering the intensity and no or few***
328 ***missed pulses across age groups and across gender.*** 67 ms is, according to Schlee (2010),
329 within the optimal perception range of the haptic receptor type Meissner corpuscle in the skin. A
330 clearly perceivable, haptic pulse for both genders is suggested to range from durations of 67 ms to
331 1000 ms.

332 • ***Force amplitudes ranging from 9 N to 18 N are recommended as they were clearly***
333 ***perceivable by all age groups for both genders.*** Similarly, as found by (Abbink and Van der
334 Helm, 2004), lower force amplitudes can be perceived better with longer durations. However, 7 N
335 is too low, independent from the combined duration. Force amplitudes stronger than 18 N should
336 be avoided, as increasing intensity of pulses turns from clear perception into a negative effect of
337 startling the driver (Edworthy and Stanton, 1995).

338 • ***Subjective perception of comfort and perceived intensity of haptic feedback can be***
339 ***influenced by gender.*** Females tended to have a higher sensitivity (higher ratings in perception)
340 and rated clear perceivable haptic pulses as less comfortable in this study.

341 • ***Shorter pulses appear more difficult to detect for older participants compared to younger***
342 ***ones (higher percentage of pulses not perceived).*** The two shortest pulse durations (20 and
343 33 ms) were the most problematic. A duration of 33 ms should be combined with high amplitudes
344 in order to be noticeable.

- 345 • **Settings might be best selected dependent on the use-case.** For an application as a warning it
346 is important that the signal is not missed, comfort is less important. A high noticeable setting with
347 no missed pulses is, for example, 67 ms combined with 18 N or 14 N, but it is perceived as not
348 comfortable. For informative use-cases comfort may be more important, therefore it could occur
349 that the signal is perceived at a repeated presentation. Such a setting would be for example, 67 ms
350 combined with 9 N, it is perceived as comfortable but a few pulses would be missed.
- 351 • ***Studies for haptic feedback should select participants counterbalanced over gender, and***
352 ***should involve older participants.***

353 **Future Research**

354 Comparable to driving on-road, engine and air conditioning produce background noise in the cabin.
355 Amongst that, the haptic pedal prototype produces a gentle sound in some settings, e.g. a squeaking
356 sound for the shortest duration pulses. The sound is not assumed to be associated with haptic
357 perception of comfort or urgency, but it could have negatively influenced the rating of intensity in two
358 ways: it could have been used as a memory aid to distinguish the pulses, or it could have been used
359 as a reference scale instead of the haptic sensation. The memory effect is assumed to be compensated
360 by random presentation order and the size of the set (16 different pulses), and six repetitive ratings
361 (each in a different random order) for each pulse. The sound as a reference scale for ratings of intensity
362 cannot be completely ruled out, but the participants were asked to focus on haptic perception, thus
363 given direction. In future, potential sound of the pedal should ideally be masked with white noise played
364 through the cabin loudspeakers.

365 A follow-up study could proceed to evaluate effects of age on the perception of intensity and comfort
366 further. It could be assessed if perception of intensity declines more in males compared to females.
367 Comfort of the haptic interface should be evaluated over a longer time. It would help to ensure that the
368 haptic feedback does not become annoying for the driver (Van Erp, 2002; Petermeijer, Abbink, Mulder,
369 and De Winter, 2015).

370 Based on the results of this study, haptic pulse feedback, which was rated as noticeable but still
371 comfortable, could be applied to a specific use-case and tested further on various on-road conditions.
372 A use-case could be a pulse as notification for exceeding a speed limit. Such a study should consider
373 various road surfaces and vehicle speeds to test the robustness of the haptic feedback. Additionally to

374 the herein presented subjective perception of the warning a future study should consider reaction time
375 as a measure and important factor for road safety. Another important consideration is to design the
376 haptic feedback such that it conveys its meaning naturally. As Norman (2002) suggests an ergonomic
377 design should not make the user (driver) think.

378 ACKNOWLEDGEMENTS

379 The authors would like to thank all volunteers for participating in the study. Support for this work was
380 provided by Engineering and Physical Sciences Research Council (EPSRC), Jaguar Land Rover and
381 WMG center HVM Catapult.

382 KEY POINTS

- 383 • Haptic pulses between 9 N and 18 N with force amplitudes longer than 33 ms were rated highly
384 noticeable. The higher in noticeability a pulse was rated the more uncomfortable it was
385 perceived (across all age groups and genders).
- 386 • When female participants rated a pulse high in intensity, they tended to rate this pulse less
387 comfortable compared to male participants.
- 388 • The subjective perception of haptic pulses delivered by an accelerator pedal to the foot was not
389 influenced by shoe type, but was significantly influenced by the pulse's duration and force
390 amplitude, as well as the participant's age and gender.

391 REFERENCES

- 392 Abbink, D. (2006). *Neuromuscular analysis of haptic gas pedal feedback during car following* (PhD Thesis). Delft
393 University of Technology, Netherlands. Retrieved from:
394 https://www.researchgate.net/publication/27348350_Neuromuscular_analysis_of_haptic_gas_pedal_feed
395 [back_during_car_following](https://www.researchgate.net/publication/27348350_Neuromuscular_analysis_of_haptic_gas_pedal_feed/back_during_car_following)
- 396 Abbink, D. & Van der Helm, F. (2004). Force perception measurements at the foot. In *Proceedings IEEE*
397 *Conference on Systems, Man and Cybernetics* (pp. 2525–2529). doi: 10.1109/ICSMC.2004.1400709
- 398 Adell, E., Várhelyi, A., & Hjälmdahl, M. (2008). Auditory and haptic systems for in-car speed management – A
399 comparative real life study. *Transportation Research Part F: Traffic Psychology and Behaviour*, 11(6),
400 445–458. doi: 10.1016/j.trf.2008.04.003
- 401 Biondi F., Rossi, R., Gastaldi, M., & Mulatti, C. (2014). Beeping ADAS: Reflexive effect on driver's behavior.
402 *Transportation Research Part F: Traffic Psychology and Behaviour*, 25(2014), 27–33.
- 403 Birrell, S., Young, M., & Weldon, A. (2013). Vibrotactile pedals: Provision of haptic feedback to support
404 economical driving. *Ergonomics*, 56(2), 282–292. doi: 10.1080/00140139.2012.760750
- 405 Brewster, S. & Brown, L. (2004). Tactons: Structured tactile messages for non-visual information display. In
406 *Proceedings of Australasian User Interface Conference, 2004* (pp. 15–23).
- 407 Brown, S. (2005). *Effects of haptic and auditory warnings on driver intersection behavior and perception* (MSc
408 Thesis). Virginia Polytechnic Institute and State University, USA. Retrieved from:
409 <http://techworks.lib.vt.edu/handle/10919/31844>

- 410 De Rosario, H., Louredo, M., Díaz, I., Soler, A., Gil, J., Solaz, J., & Jornet, J. (2010). Efficacy and feeling of a
411 vibrotactile frontal collision warning implemented in a haptic pedal. *Transportation Research Part F: Traffic*
412 *Psychology and Behaviour*, 13(2), 80–91. doi: 10.1016/j.trf.2009.11.003
- 413 Edworthy, J. & Stanton, N. (1995). A user-centred approach to the design and evaluation of auditory warning
414 signals: 1. Methodology. *Ergonomics*, 38(11), 2262-2280. doi: 10.1080/00140139508925267
- 415 Geitner, C., Birrell, S., Skrypchuk, L., Krehl, C., & Jennings, P. (2015). Good vibrations – Driving with a haptic
416 pedal. In *Proceedings of the AutomotiveUI '15 Conference*, Nottingham, UK.
- 417 Hale, K. & Stanney, K. (2004). Deriving haptic design guidelines from human physiological psychophysical, and
418 neurological foundations. *Computer Graphics and Applications, IEEE*, 24(2), 33-39. doi:
419 10.1109/MCG.2004.1274059
- 420 Halonen, P. (1986). Quantitative vibration perception thresholds in healthy subjects of working age. *European*
421 *Journal of Applied Physiology and Occupational Physiology*. 54(6), 647-655. doi: 10.1007/BF00943355
- 422 Hennig, E. & Sterzing, T. (2009). Sensitivity mapping of the human foot: Thresholds at 30 skin locations. *Foot*
423 *Ankle International*, 30(10), 986-91. doi: 10.3113/FAI.2009.0986
- 424 Hilz, M., Axelrod, F., Hermann, K., Haertl, U., Duetsch, M., & Neundörfer, B. (1998). Normative values of
425 vibratory perception in 530 children, juveniles and adults aged 3–79 years. *Journal of the Neurological*
426 *Sciences*, 159(2), 219-225. doi: http://dx.doi.org/10.1016/S0022-510X(98)00177-4
- 427 Ichinose, A., Gomikawa, Y., & Suzuki, S. (2013). Driving assistance through pedal reaction force control with
428 consideration of JND. In *RO-MAN, 2013 IEEE*, (pp. 484–489). doi: 10.1109/ROMAN.2013.6628551
- 429 Inglis, J., Kennedy, P., Wells, C., & Chua, R. (2002). The role of cutaneous receptors in the foot. *Advances in*
430 *Experimental Medicine and Biology*, 508(2002), 111-117. doi: 10.1007/978-1-4615-0713-0_14
- 431 Kaaresoja, T. & Linjama, K. (2005). Perception of short tactile pulses generated by a vibration motor in a mobile
432 phone. In *Proceedings of World Haptics* (pp. 471-472), IEEE Press. doi: 10.1109/WHC.2005.103
- 433 Kennedy, P. & Inglis, J. (2002). Distribution and behaviour of glabrous cutaneous receptors in the human foot
434 sole. *The Journal of Physiology*, 538(3), 995–1002. doi: 10.1113/jphysiol.2001.013087
- 435 Lee, J., Hoffman, J., & Hayes, E. (2004). Collision warning design to mitigate driver distraction. In *Proceedings of*
436 *the SIGCHI conference on Human Factors in Computing Systems* (pp. 65-72). ACM Press. doi:
437 10.1145/985692.985701
- 438 MacLean, K. & Enriquez, M. (2003). Perceptual design of haptic icons. In *Proceedings of the Eurohaptics* (pp.
439 351-363), Dublin, Ireland.
- 440 Mehler, B., Reimer, B., & Coughlin J. (2011). Sensitivity of physiological measures for detecting systematic
441 variations in cognitive demand from a working memory task: An on-road study across three age groups.
442 *Human Factors*, 54(3), 396-412. doi: 10.1177/0018720812442086
- 443 Neely, G., Burström, L., & Johansson, M. (2001). Subjective responses to hand-arm vibration: Implications for
444 frequency-weighting and gender differences. In *Proceedings of the 17th Annual Meeting of the*
445 *International Society of Psychophysics* (pp. 553–558).
- 446 Norman, D. (2002). *The Design of Everyday Things*. New York, USA: Basic Books.
- 447 Petermeijer, S., Abbink, D., Mulder, M., & De Winter, J. (2015). The effect of haptic support systems on driver
448 performances: A literature survey. *IEEE Transactions on Haptics*, 8(4), 467-479. doi:
449 10.1109/TOH.2015.2437871
- 450 Perry, S. (2006). Evaluation of age-related plantar-surface insensitivity and onset age of advanced insensitivity in
451 older adults using vibratory and touch sensation tests. *Neuroscience Letters*, 392: 62–67. doi:
452 10.1016/j.neulet.2005.08.060
- 453 R Core Team. (2014). *R: A Language and Environment for Statistical Computing*. Vienna, Austria. Retrieved from
454 <http://www.R-project.org/>
- 455 Schlee, G. (2010). *Quantitative assessment of foot sensitivity: The effects of foot sole skin temperature, blood*
456 *flow at the foot area and footwear* (PhD Thesis). Technische Universitaet Chemnitz, Germany.
- 457 Shaffer, S. & Harrison, A. (2007). Aging of the somatosensory system: A translational perspective. *Physical*
458 *Therapy*. 87(2), 193-207. doi: 10.2522/ptj.20060083
- 459 Travieso, D. & Lederman, S. (2007). Assessing subclinical tactual deficits in the hand function of diabetic blind
460 persons at risk for peripheral neuropathy. *Archives of Physical Medicine and Rehabilitation*, 88(12), 1662-
461 72. doi: 10.1016/j.apmr.2007.09.007
- 462 Van Erp, J. (2002). Guidelines for the use of vibro-tactile display in human computer interaction. In *Proceedings*
463 *of Eurohaptics 2002* (pp. 18-22), Edinburgh, UK, University of Edinburgh.
- 464 Verrillo, R. (1982). Effects of aging on the suprathreshold responses to vibration. *Perception & Psychophysics*,
465 32(1), 61-68. doi: 10.3758/BF0320486