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Quantum limits of localisation microscopy

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Abstract

Localisation microscopy of multiple weak, incoherent point sources with possibly different intensities in one spatial dimension is equivalent to estimating the amplitudes of a classical mixture of coherent states of a simple harmonic oscillator. This enables us to bound the multi-parameter covariance matrix for an unbiased estimator for the locations in terms of the quantum Fisher information matrix, which we obtained analytically. In the regime of arbitrarily small separations we find it to be no more than rank two—implying that no more than two independent parameters can be estimated irrespective of the number of point sources. We use the eigenvalues of the classical and quantum Fisher information matrices to compare the performance of spatial-mode demultiplexing and direct imaging in localisation microscopy with respect to the quantum limits.

1. Introduction

Precisely locating multiple single emitters is a key challenge in fluorescence microscopy. The process of estimating these locations depends on the quality of the image obtained by the microscope. One of the major limitations to the image quality, known since Abbe and Rayleigh, lies in spatially resolving objects substantially smaller than half the wavelength of the light involved [1]. Known as the Rayleigh limit or diffraction limit, it is a consequence of the diffraction of light due to its wave nature.

Over the last couple of decades, ways to circumvent the Rayleigh limit in far-field fluorescence microscopy have been invented [2]. Confocal methods such as STED, RESOLFT, and SSIM [3–6] use patterned illumination to spatially modulate the fluorescence pattern of emitters within a diffraction-limited region such that not all of them emit simultaneously, thereby achieving sub-Rayleigh resolution. Other far-field methods such as PALM, fPALM and STORM [7–9] temporally modulate the fluorescence pattern of emitters with weak laser pulses stochastically such that only a low density of emitters are active within the Rayleigh limit at one time. Repeating the process many times, images with sub-Rayleigh resolution are reconstructed from the measured positions of individual emitters. These techniques, with resolution of tens of nanometers, have provided insights into biological processes at the cellular scale that were hitherto unattainable [10].

Though immensely powerful and impressive, none of these methods seek to extract all the information available in the emitted light field. As in conventional fluorescence microscopy these techniques use ‘direct imaging’—intensity measurements on the image plane—to extract information from the incident light. That there is indeed more information in the light field to be extracted was shown by Tsang et al [11]. Using methods from classical and quantum estimation theory, it was shown theoretically that two arbitrarily close incoherent point sources may be resolved, and that this may be achieved in practice using a spatial-mode demultiplexing (SPADE) measurement. In the few years since, theoretical studies have considered different source arrangements or parameters of interest [12–17] in one as well as in two and three spatial dimensions [18–21].

Other theoretical studies have explored various detection systems that could achieve the ultimate precision in imaging or get close to it [22–25]. Several experiments have demonstrated some of the principles underlying these detection systems [26–33]. Advances in this area have been recently reviewed by Tsang [34].

Realistic imaging scenarios typically involve more than two point sources or even extended objects. It has been shown that an extended one-dimensional object much smaller than the Rayleigh limit described only in
terms of its centroid and effective radius can be approximated by a two-level quantum system [15]. Theoretical optimality of certain measurement techniques in estimating this effective radius size has also been established in one and two spatial dimensions [17, 35, 36]. Order-of-magnitude bounds on the precision of estimating the normalised moments of extended sources smaller the Rayleigh limit have also been obtained [36, 37].

In this paper, we provide an analytical lower bound on an unbiased estimator’s covariance (mean square error) matrix for localisation microscopy—simultaneously estimating the locations of N incoherent, weak point sources of unequal but known intensities in one spatial dimension. The bound is provided by the the quantum Fisher information matrix (QFIM). For a Gaussian point spread function (PSF), we first describe the light field on the image plane as a classical mixture of coherent states. We use this to derive the QFIM analytically. In the limit of the point sources approaching a single point, we find its rank to be no more than two. As the inverse of the QFIM lower bounds the covariance matrix, our result implies that no more than two independent parameters can be estimated in localisation microscopy in the limit of arbitrarily small separations. In this limit, we provide a mathematical explanation for our observation in terms of an approximation of the light field involving only the first two Hermite–Gauss modes. Finally, we compare performance of conventional direct imaging and the recently proposed SPADE [11] in localisation microscopy with the quantum bounds we obtain. For the subset of parameters where scalings may be optimal, we find SPADE to be short of the quantum limit in absolute precision.

This paper is organised as follows: in section 2 we provide a quantum mechanical description of localisation microscopy. The appropriate framework to study the quantum limits of the localisation problem is quantum estimation theory, the toolbox of which is described in section 3, leading to the definition of the QFIM. In section 4 we provide an analytic expression of the QFIM for localisation microscopy, our main technical result. We then draw conclusions about its rank and its implications for localisation microscopy. We end in section 5 with further insights and discussions about the sinc PSF and the potential of detection systems attaining the quantum limits of localisation microscopy.

2. Quantum description of localisation microscopy

We consider localisation microscopy—the problem of estimating the locations of N incoherent point sources or emitters located in a one-dimensional spatial configuration as in figure 1. As we assume them to be weak, such that on average no photons arrive on the image plane within a coherence time with probability \((1 - \epsilon)\), where \(\epsilon \ll 1\) and one photon arrives with probability \(\epsilon\). We also assume the optical field on the image plane to be quasi-monochromatic and paraxial [11]. The quantum state of this optical field is then

\[
\rho_{\text{opt}} \approx (1 - \epsilon) \rho_{\text{vac}} + \epsilon \rho,
\]

where we have neglected terms of second and higher orders in \(\epsilon\) and \(\rho_{\text{vac}} = |\text{vac}\rangle \langle \text{vac}|\) is the vacuum state and \(\rho\) is the one-photon state.

![Figure 1. Illustration of localisation microscopy with five point sources, imaged by a diffraction-limited system and the resultant intensity distribution on the image plane.](image-url)
The one-photon density matrix on the object plane is an incoherent mixture of position eigenstates
\[ \rho = \sum_{i=1}^{N} w_i |\chi_i\rangle \langle \chi_i|, \]
where \( w_i \) are the relative intensities with \( \sum_{i=1}^{N} w_i = 1 \). An imaging system maps \( \hat{\varepsilon}_i^a \), the creation operator producing one photon in the position \( x \) on the object plane, to the corresponding image plane operator \( \hat{\varepsilon}_i^b \) [13]
\[ \hat{\varepsilon}_i^b = \int dx \psi_{\text{PSF}}(x - \chi_i) \hat{\varepsilon}_x^i, \]
where \( \chi_i \) is the position on the source on the object plane and \( \psi_{\text{PSF}}(x) \) is the PSF. On the image plane this becomes
\[ \rho = \sum_{i=1}^{N} w_i |\psi_i\rangle \langle \psi_i|, \]
where
\[ |\psi_i\rangle = \int dx \psi_{\text{PSF}}(x - \chi_i) |x\rangle, \]
as follows from equation (2).

An ideal imaging system with \( \psi_{\text{PSF}}(x) = \delta(x) \) is free of any Rayleigh limit as it transmits all spatial frequencies from the object to the image plane. In practice, a Gaussian PSF
\[ \psi_{\text{PSF}}(x) = \frac{1}{(2\pi\sigma^2)^{1/4}} e^{-x^2/(4\sigma^2)}, \]
with \( \sigma = \lambda/(2\pi N\text{A}) \), where \( N\text{A} \) is the numerical aperture of the imaging system is a good approximation for quasimonochromatic paraxial light [11, 38] and also allows us to obtain analytical results. For such a PSF, the state of equation (3) has an intensity distribution of the form illustrated in figure 1. For a Gaussian PSF, the \( |\psi_i\rangle \) can be expanded in the HG basis as (see appendix A)
\[ |\psi_i\rangle = \sum_{k=0}^{\infty} \frac{\alpha_i^k}{\sqrt{k!}} e^{-\alpha_i^2/2} |\phi_k\rangle \equiv |\alpha_i\rangle, \]
where \( |\phi_k\rangle \) are the HG modes\(^2\). This has the same mathematical form as the coherent states, produced by the displacement operator \( D(\alpha_i) = e^{\alpha_i a^\dagger - \alpha_i^* a} \) [39] acting on the ground state of the harmonic oscillator with \( \alpha_i = \chi_i/2\sigma \in \mathbb{R} \) the dimensionless positions of the sources. Thus the one-photon state on the image plane is
\[ \rho \equiv \rho_\alpha = \sum_{i=1}^{N} w_i |\alpha_i\rangle \langle \alpha_i|, \]
a classical mixture of coherent states in the HG basis.

The above is a quantum optical rendition of localisation microscopy—a classical optics problem. It enables us to harness the mathematical formalism associated with coherent states and provides a basis that spans the space of the quantum state as well as its derivative. The latter is an essential ingredient of deriving the QFIM analytically in section 4.1. We also hope that this description will provide insights into the quantum limits to localisation microscopy in the presence of shot noise and assist in designing detection systems that attain these quantum limits.

### 3. Quantum estimation theory

Localisation has long been treated as an estimation problem with the unknown locations of the sources \( \chi \equiv \{ \chi_i \}, \quad i = 1, \ldots, N \) being the parameters to be estimated [40, 41]. In our formulation, the limits to the localisation of the point sources are the same as estimating the amplitudes \( \alpha \equiv \{ \alpha_i \}, \quad i = 1, \ldots, N \) of the coherent states in equation (7). Let these estimates be \( \hat{\alpha} \equiv \{ \hat{\alpha}_i \} \). The precision of our estimate is then given by the covariance (or mean square error) matrix defined as
\[ \text{Cov}\{\alpha\} = \sum_{z} p(z|\alpha)(\alpha - \hat{\alpha})(\alpha - \hat{\alpha})^T, \]
where \( p(z|\alpha) \) is the probability distribution of the collected data labelled by, for instance, the pixel \( z \) on the image plane. \( \text{Cov}\{\alpha\} \) is a positive symmetric matrix whose \( ith \) diagonal element denotes the variance of an estimator of \( \alpha_i \) given the data collected. The \((i,j)\)th off-diagonal element denotes the covariance in the estimation of \( \alpha_i \) and \( \alpha_j \).

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\(^2\) Unlike the conventional quantum optical coherent states which reside in the phase space of the electromagnetic field, our coherent states reside in physical space on the image plane. This mathematical form was also identified by Dutton et al [17] but only used for numerical calculations.
Given the data collected, the maximum amount of information that can be extracted from it to obtain the most precise estimate of the locations is given by the Cramér–Rao bound [42]. For an unbiased estimator, this bound is given by

\[ \text{Cov}[\alpha] \geq \frac{1}{M} |C(\rho_\alpha, \Pi_z)|^{-1}, \]  

where \( M \) is the number of coherence times over which the data is collected, making \( Me \) the total photon count. This inequality is saturable but generally only in the asymptotic limit of many repetitions [43]. \( C(\rho_\alpha, \Pi_z) \) is the CFIM whose elements are given by [44]

\[ [C(\rho_\alpha, \Pi_z)]_{\mu\nu} = \sum_z \frac{1}{p(z|\alpha)} \frac{\partial p(z|\alpha)}{\partial \alpha_{\mu}} \frac{\partial p(z|\alpha)}{\partial \alpha_{\nu}}. \]  

The probability distribution \( p(z|\alpha) = \text{Tr} (\rho_\alpha \Pi_z) \) results from detecting the light on the image plane using a specific detection system \( \Pi_z \). Fluorescence microscopy typically employs intensity detectors \( \Pi_z = \{|n\rangle \langle n| \}, \quad n = 0, 1, \cdots \) at each pixel \( z \), known as direct imaging. It is then evident that the CFIM depends on the detection system used, and not surprising that it determines the amount of information that can be extracted from the light field at the image plane.

To identify the quantum limit on the precision of localisation microscopy, the CFIM must be maximised over all possible physically allowed detection systems. This set is given by positive operator-valued measures (POVMs) [45] and the maximisation is bounded as [46, 47],

\[ \max_{[\Pi_z]} C(\rho_\alpha, \Pi_z) \leq Q(\rho_\alpha), \]  

by the QFIM. Its matrix elements are given by

\[ [Q(\rho_\alpha)]_{\mu\nu} = \text{Tr} \left[ \rho_\alpha L_\mu^\alpha L_\nu^\alpha + L_\nu^\alpha L_\mu^\alpha \right], \]  

with \( L_\alpha \) being the symmetric logarithmic derivative (SLD) corresponding to the parameter \( \alpha_\mu \). The SLD is determined by the Lyapunov equation

\[ 2 \frac{\partial \rho_\alpha}{\partial \alpha_\mu} = (\rho_\alpha L_\mu + L_\mu^\alpha \rho_\alpha). \]  

The quantum limit to localisation microscopy is thus given by

\[ \text{Cov}[\alpha] \geq \frac{1}{M} |C(\rho_\alpha, \Pi_z)|^{-1} \geq \frac{1}{M} |Q(\rho_\alpha)|^{-1}. \]  

The QFIM depends only on the light field on the image plane and determines the maximum amount of information that can be extracted from it using detection systems allowed by quantum mechanics. Deriving an analytical expression for \( Q(\rho_\alpha) \) for state in equation (7) is our main result, which we present in the next section.

A practical issue following the identification of the quantum limit is its attainability. For cases where a single parameter is unknown then a measurement can be found to satisfy the equality of equation (11), which involves projecting onto the eigenstates of the SLD [44, 48]. However this strategy does not generalise to multiple parameters, as in localisation microscopy, in general.

For multi-parameter estimation the attainability is tantamount to saturating the second inequality in equation (14). A necessary condition for the saturability of any scalar form of equation (14) is the satisfaction of weak commutativity [49, 50],

\[ \text{Tr}(\rho_\alpha [L^\mu, L^\nu]) = 2 \text{Tr}(\text{Im}(\rho_\alpha L^\mu L^\nu)) = 0. \]  

Moreover, through the quantum theory of asymptotic normality [51], this condition becomes sufficient with the application of collective measurements over multiple copies of \( \rho_\alpha \) [49, 50].

Any scalar function of the covariances can be bounded by the inverse of QFIM with the lower bound following from the spectral decomposition of QFIM. To that end, calculating the eigenvalues of the QFIM and their scaling is of importance for the multi-parameter estimation. For localisation microscopy, \( \rho_\alpha \) as in equation (7) as well as its derivative are real matrices. Thereby, \( L^\mu, L^\nu \) are also real and the above condition is always satisfied. The quantum limit for localisation microscopy is therefore attainable, at least in principle, although collective measurements over multiple copies [49, 50] of the light field on the image plane may be required.

Alternative parameterisations of the system—where the new parameters \( \alpha' \) are functions of the old parameters \( \alpha \)—can be dealt with by a transformation of the QFIM. Given the transformation matrix \( B \) with

\[ \text{since the density matrix and its derivatives are real-valued in the orthonormal \{\phi_i\} basis, equation (13) is a system of equations with real coefficients. Hence } \]
elements $B_{ij} = \partial \alpha_i / \partial \alpha'_j$, the QFIM of the transformed parameters is [44]

$$Q' = B \bar{Q} B^T,$$

(16)

provided the transformation is non-singular. This can be used to recast our results in terms of, for instance, the moments of the point source distribution.

4. Results

We now present our main result—the analytical expression of the QFIM for localisation microscopy. This expression allows us to conclude that the QFIM is a rank two matrix as $\alpha_i \rightarrow 0$. Equation (14) then implies that the eigenvalues of $\text{Cov} [\alpha]$ remains finite for no more than two independent parameters. Thus, no more than two independent parameters can be estimated from the entire set $\alpha$ as $\alpha \rightarrow 0$.

We lack a fully satisfactory physical explanation for this restriction on the number of estimable parameters, but provide an explanation involving only the first two HG modes for $\alpha_i \ll 1$.

4.1. Analytical expression of QFIM

The state in equation (7) can be expressed in the basis of $\{|\alpha_1\}, \{|\alpha_2\}, \{|\alpha_N\}\}$ as

$$\rho_\alpha = A \begin{pmatrix} D_\alpha & 0 \\ 0 & 0 \end{pmatrix} A^\dagger \equiv A \rho_A A^\dagger,$$

(17)

where $A = (|\alpha_1\rangle \langle \alpha_2| \cdots |\alpha_N\rangle \langle \alpha_1| \cdots \langle \alpha_N|)$

(18)

and $D_\alpha = \text{diag}(\eta_1, \eta_2, \cdots, \eta_N)$ denotes a diagonal matrix. Although the basis used in equation (17) is non-orthogonal this representation can still be used to evaluate the QFIM [52]. The coherent states $|\alpha_i\rangle$ are linearly independent and span the support of the state in equation (7). The support of the derivative is spanned by $|\alpha_i\rangle$ and $|\alpha_i\rangle$, which are also linearly independent.

The Grammian matrix

$$\Upsilon = A^\dagger A,$$

(19)

whose elements consist of the scalar products between the basis vectors $\langle \alpha_i|\alpha_k\rangle$, $\langle \alpha_j|\alpha_k\rangle$, $\langle \alpha_i|\alpha_j\rangle$, and $\langle \alpha_i|\alpha_j\rangle$ is in block form,

$$\Upsilon = \begin{pmatrix} \Upsilon_{\alpha\alpha} & \Upsilon_{\alpha d} \\ \Upsilon_{d\alpha} & \Upsilon_{dd} \end{pmatrix},$$

(20)

where

$$\Upsilon_{\alpha\alpha}(\alpha) = \langle \alpha_i|\alpha_j\rangle = e^{-(\alpha_i - \alpha_j)^2 / 2},$$

$$\Upsilon_{\alpha d}(\alpha) = \langle \alpha_i|\alpha_j\rangle = \alpha_i e^{-(\alpha_i - \alpha_j)^2 / 2} = (D_\alpha \Upsilon_{\alpha\alpha})(\alpha),$$

$$\Upsilon_{d\alpha}(\alpha) = \langle \alpha_i|\alpha_j\rangle = \langle \alpha_i\alpha_j + 1 \rangle e^{-(\alpha_i - \alpha_j)^2 / 2}$$

(21)

and $D_\alpha = \text{diag}(\alpha_1, \alpha_2, \cdots, \alpha_N)$.

Since $\partial_\alpha|\alpha\rangle = (\hat{a}_\alpha - \alpha)|\alpha\rangle$ for real $\alpha$, the derivative of the quantum state is

$$\partial_\alpha \rho_\alpha = A \begin{pmatrix} -2\alpha_j \delta_j & E_j \\ E_j & 0 \end{pmatrix} A^\dagger \equiv A (\partial_\alpha \rho_A) A^\dagger,$$

(22)

where $\partial_\alpha$ denotes the derivative with respect to $\alpha_j$ and $(E_j)_{\alpha\beta} = \delta_{\alpha \beta} \delta_j$. Similarly, the SLD $L_A^j$ can be written in the generic form

$$L_A^j = A L_A^{j\alpha} A^\dagger = A \begin{pmatrix} L_A^{j\alpha} & L_A^{j d} \\ L_A^{d\alpha} & L_A^{d d} \end{pmatrix} A^\dagger,$$

(23)

where $L_A^{j\alpha}$ corresponds to the elements $\langle \alpha_i| L_A^j |\alpha_j\rangle$, $L_A^{j d}$ to $\langle \alpha_i| L_A^d |\alpha_j\rangle$ etc. The Lyapunov equation equation (13) can be now rewritten as

$$2 \partial_\alpha \rho_\alpha = \rho_\alpha \Upsilon L_A^j + L_A^j \rho_\alpha,$$

(24)

and the QFIM elements from equation (12) as

$$[\mathcal{Q}(\rho_\alpha)]_{jk} = \text{Tr} (\partial_\alpha \rho A L_A^j) = \text{Tr} (\partial_\alpha \rho_A L_A^j \Upsilon),$$

(25)
Using the Tracy–Singh block kronecker product \( \odot \) and the block column ‘vecb’ operator [53] defined as
\[
\text{vecb}(L_j) = \begin{bmatrix} L_{j,xx} \\ L_{j,xd} \\ L_{j,dd} \\ L_{j,dd} \end{bmatrix},
\]
(26)
where \([X] = \text{vec}(X)\) is the column vectorisation of a matrix and \((X)\) its transpose. Equation (24) can be blockwise vectorised to
\[
2\text{vecb}(\partial_j \rho_\alpha) = (\mathbb{I} \odot (\rho_\alpha T) + (\rho_\alpha T) \odot \mathbb{I}) \text{vecb}(L_j)
\]
(27)
with \(\mathbb{I}\) being the identity matrix. Using the matrix identity [53]
\[
\text{Tr} (A^T B C D^T) = \text{vecb}(A^T) (D \odot B) \text{vecb}(C),
\]
the QFIM elements from equation (25) can be re-expressed as
\[
[Q(\rho_\alpha)]_{ij} = \text{vecb}(\partial_i \rho_\alpha)^T (T \odot T) \text{vecb}(L_j) = w_i - 2\alpha_i \langle E_i \rangle \langle E_i \rangle \langle E_i \rangle \langle E_i \rangle \begin{bmatrix} \Gamma_{i,xx}^j \\ \Gamma_{i,xd}^j \\ \Gamma_{i,dd}^j \end{bmatrix},
\]
(29)
where we have defined
\[
(T \odot T) \text{vecb}(L_j) = \text{vecb}(\Gamma^j) = \begin{bmatrix} \Gamma_{i,xx}^j \\ \Gamma_{i,xd}^j \\ \Gamma_{i,dd}^j \end{bmatrix}
\]
(30)
which is the outstanding quantity to be determined.

We now recast equations (27) and (29) as
\[
2\text{vecb}(\partial_j \rho_\alpha) = (T^{-1} \odot \rho_\alpha + \rho_\alpha \odot T^{-1}) (T \odot T) \text{vecb}(L_j)
\]
\[
= (T^{-1} \odot \rho_\alpha + \rho_\alpha \odot T^{-1}) \text{vecb}(\Gamma^j).
\]
(31)
Putting it all together, we obtain
\[
\begin{bmatrix} -4w_i \alpha_i \langle E_i \rangle \\ 2w \langle E_i \rangle \\ 2w \langle E_i \rangle \\ 0 \end{bmatrix} = \begin{bmatrix} \mathbb{A} & 0 \\ 0 & \mathbb{A} \\ 0 & 0 \\ 0 & 0 \end{bmatrix} \begin{bmatrix} \Gamma_{i,xx}^j \\ \Gamma_{i,xd}^j \\ \Gamma_{i,dd}^j \end{bmatrix},
\]
(32)
where
\[
\mathbb{A} = \begin{bmatrix} D_w \otimes \nu_{xx} + \nu_{xx} \otimes D_w \\ D_w \otimes \nu_{xd} + \nu_{xd} \otimes D_w \\ D_w \otimes \nu_{dd} + \nu_{dd} \otimes D_w \\ 0 & 0 & 0 & 0 \end{bmatrix}
\]
(33)
and \([\nu_{xx}, \nu_{xd}, \nu_{dd}, \nu_{dd}]\) defines the inverse of \(T\) via
\[
T^{-1} = \begin{bmatrix} \nu_{xx} & \nu_{xd} \\ \nu_{xd} & \nu_{dd} \end{bmatrix}
\]
(34)
Note that the inverse \(T^{-1}\) always exists since \(T\) is the Grammian matrix of linearly independent vectors. The elements of \(T^{-1}\) can be found using the formula of blockwise inversion (see appendix B).

Noticing that \(\Gamma_{i,dd}^j\) does not contribute in equation (29), equation (32) can be reduced to
\[
\begin{bmatrix} -4w_i \alpha_i \langle E_i \rangle \\ 2w \langle E_i \rangle \\ 2w \langle E_i \rangle \end{bmatrix} = \mathbb{A} \begin{bmatrix} \Gamma_{i,xx}^j \\ \Gamma_{i,xd}^j \end{bmatrix},
\]
(35)
where \(\mathbb{A}\) is a \(3N^2 \times 3N^2\) invertible matrix unless \(\alpha_i = \alpha_j\) for some \(i, j\), which is a singular case for which the rank of the density matrix reduces. Hence the unique solution to equation (35) is
where the block matrices that compose the \( \mathcal{K}^{-1} \) can be found by using the formulas for blockwise inversion (see appendix B).

Substituting equation (36) into (29) gives us the QFIM elements

\[
\left[ \begin{array}{c}
\Gamma_{\alpha\alpha}^j \\
\Gamma_{\alpha\beta}^j \\
\Gamma_{\beta\beta}^j
\end{array} \right] = \mathcal{K}^{-1} \left[ \begin{array}{c}
-4w_j \alpha_j |E_j| \\
2w_j |E_j| \\
2w_j |E_j|
\end{array} \right],
\]

where the block matrices that compose the \( \mathcal{K}^{-1} \) can be found by using the formulas for blockwise inversion (see appendix B).

Figure 2. Diagonal and off-diagonal elements of the QFIM for the case of 3 sources with equal intensities. The sources are separating from each other at equal distances, \((\alpha_1, \alpha_2, \alpha_3) = (x, 2x, 3x)\). The element \( Q_{11} \) and \( Q_{13} \) elements are equal, as are the \( Q_{11} \) and \( Q_{33} \) elements.

\[
\begin{align*}
Q_{11} & = Q_{13} \\
Q_{12} & = Q_{23} \\
Q_{22} & = Q_{33}
\end{align*}
\]

We have explicitly checked this for \( N = 4, \ldots, 10 \) as well as when the sources are not equally spaced. In figure B1 in appendix B we plot the eigenvalues of the QFIM for \( N = 4, 5 \) as further examples. In the case of different relative intensities the results are the same except of the limiting case of one extremely bright source \( w_j \gg 1 \), \( w_{i\neq j} \ll 1 \) where the rank of the QFIM is approximately one (figure B2 in appendix B).

Since the QFIM has rank two as \( x \to 0 \), its inverse is ill-defined except on a two-dimensional subspace. This implies that the \( N \times N \) covariance matrix for localisation microscopy, as per equation (14), will also be unbounded except on a two-dimensional subspace. Thus, no more than two independent parameters can be estimated in localisation microscopy as the point sources approach each other.

In other words, the rank-deficient nature of the QFIM shows that a form of the Rayleigh limit resurfaces for any \( N > 2 \). This had been suggested by previous works based on order-of-magnitude bounds for the diagonal elements on the CFIM [36] or upper bounds on the diagonal elements of the QFIM [37]. Our analytical expression for the full QFIM—its diagonal and off-diagonal elements for any \( N \)—shows that this rank two behaviour is truly quantum mechanical in origin. Furthermore, knowing the full QFIM matrix allows us to uncover the nature in which \( N = 2 \) of the eigenvalues approach zero. We return to the behaviour in which this rank deficiency or Rayleigh limit emerges in section 5.
4.2. Why rank two?
We now provide an explanation for the rank deficiency of the QFIM in the regime of small separations which can be seen as the re-emergence of the Rayleigh limit. To that end, we express the state in equation (7) in terms of the real-valued displacement operator $\hat{a} = \hat{a} - \Delta e^{i \chi}$ as

$$\rho = \sum_i \sqrt{\omega_i} \hat{D}(\alpha_i) |0\rangle \langle 0| \sqrt{\omega_i} \hat{D}^\dagger(\alpha_i).$$

In the limit of very small separations ($\alpha_i \ll 1$), the displacements are approximately

$$\hat{D}(\alpha_i) = \mathbb{I} + \alpha_i (\hat{a}^\dagger - \hat{a}) + \mathcal{O}(\alpha_i^2),$$

where $\mathbb{I}$ is the identity operator and the displacement $\alpha_i$ is real. Up to the second order in $\alpha_i$, the normalised quantum state of the light field on the image place is then

$$\rho^{(2)} = \begin{pmatrix} 1 - C_2 & C_1 \\ C_1 & C_2 \end{pmatrix},$$

where $C_i$ are the first two moments

$$C_1 = \sum_{i=1}^N w_i \alpha_i, \quad C_2 = \sum_{i=1}^N w_i \alpha_i^2.$$

Equation (40) describes the state of two-level quantum system—the two levels being the first two HG modes. A similar approximation which described the state relative to a PSF centred at a fixed reference point was used in reference [15] to estimate the centroid and the effective radius of a distribution of incoherent point sources. We now consider the more general problem of estimating the location of $N$ point sources.

The QFIM for $\alpha$ (see appendix C) is

$$\mathcal{Q}(\rho^{(2)}_\alpha) \equiv \mathcal{I} = \frac{1}{\mathcal{A}} (\mathbb{I} - \alpha \mathcal{M}) \mathcal{M}^{-1} \mathcal{M}^\dagger,$$

with

$$\mathcal{M} = \begin{bmatrix} M_{11} & M_{12} \\ M_{21} & M_{22} \end{bmatrix},$$

where $M_{11} = (C_2 - 1) C_2$, $M_{12} = M_{21} = C_1 - 2 C_2$, $M_{22} = 4 C_2^2 - 1$, $\mathcal{A} = (C_2 - 1) C_2 + C_2^2$, and $\mathbb{I} = (1 \ldots 1)^T$.

The QFIM $\mathcal{I}$ is an $N \times N$ matrix, which is a product of three matrices of dimensions $N \times 2, 2 \times 2$ and $2 \times N$. Since $\text{rank}(AB) \leq \min \{\text{rank}(A), \text{rank}(B)\}$, and the matrix $\mathcal{M}$ has rank 2, the QFIM $\mathcal{I}$ has rank no more than two. Although a two-level quantum system has the potential of estimating three real parameters, localisation microscopy in this limit can estimate only two as the two-level system possesses a real density matrix. This is another way of arguing that as the point sources get closer, the light field on the image plane has

Figure 3. The eigenvalues of the QFIM matrix for 3 sources with equal intensities. The sources are separating from each other at equal distances, $(\alpha_1, \alpha_2, \alpha_3) = (x, 2x, 3x)$.

4 As the localisation parameters $\alpha$ are real, $\text{Tr}(\rho^{(2)}_\alpha \sigma_y) = 2 \text{Im}(C_2) = 0$, where $\sigma_y$ is the Pauli Y matrix.
enough information to estimate only two parameters. A physical reason for this observation would be highly desirable.

5. Discussion

Our analytical expression for the QFIM for localisation microscopy has enabled us to show that as point sources get closer, no more than two independent parameters can be estimated. A rank-deficient QFIM occurs when the quantum state does not contain enough information to permit the estimation some of the parameters or combinations thereof. The parameters that can be estimated correspond to the non-zero eigenvalues of the QFIM. Without additional knowledge of the source distribution this restricts us to estimating functions of the first two moments only deep in the sub-Rayleigh limit. As equation (42) shows, when all \( \{ \alpha_j \} \) are unknown as in localisation microscopy, there is vanishing information about any single \( \alpha_i \) itself. This is in contrast to the scalar QFI \( r(\alpha_i) \) which is non zero, but assumes that all the other \( \{ \alpha_j \} \) are known.

The manner in which the eigenvalues of the QFIM tend to zero is of interest in the search for optimal detection systems for localisation microscopy. Numerical fitting in figure 4 shows the vanishing eigenvalues of the QFIM approach zero polynomially. The degree of the polynomial is given by \( \mu = m - d^2 + 1 \), where \( \mu \) is the order the eigenvalue when arranged in descending order and \( \lfloor \cdot \rfloor \) is the floor function. These scalings are now extracted from the elements of the full QFIM of the localisation parameters \( a \)—rather than from bounds on estimating the various moments independently as in previous works [36, 37].

Unlike the latter, we can now compare the absolute performance of detection systems for localisation microscopy relative to its quantum limit. Indeed, while figure 5 shows the 2nd eigenvalue of the QFIM closely parallel to the nth eigenvalue of the CFIM for SPADE [11], there is a large gap in the absolute terms. This could be due to the sub-optimality of SPADE for estimating the \( N/2 \) parameters it is sensitive to. Similar scalings were observed with detection using superpositions of the conventional SPADE basis [35–37] that are sensitive to the other half of the moments. For reference over a range of separations, figure E1 in appendix E shows the eigenvalues of the CFIM for SPADE as well as direct imaging. Note that for both, the CFIM tends towards a rank one matrix.

Finally, although our analytical result is derived with a Gaussian PSF, we expect the rank deficiency of the QFIM to be present in a more general family of PSFs. To that end, figure 6 shows the numerically obtained eigenvalues of the QFIM for three equidistant point sources of equal intensities under a sinc PSF (see appendix D) defined as

\[ r(\alpha_i) = \frac{1}{2} \left\lfloor \frac{\alpha_i}{\pi} \right\rfloor \]

5 Conventional SPADE is not sensitive to all the parameters needed to describe the sources' distribution, only its even moments [34, 37, 38].
This PSF is the exact form for diffraction through a sharp one-dimensional slit which in its principal peak is well-approximated as Gaussian.

An approximation involving the first two spherical Bessel modes as in section 4.2 can be performed for a sinc PSF as well, leading to similar insights. A proof of this rank deficiency for arbitrary PSFs and a physical explanation remains an open question.

To conclude, we have obtained several insights into the quantum limits of localisation microscopy via an analytical expression for the QFIM. In particular, the behaviour of the eigenvalues of the QFIM deep in the sub-Rayleigh limit revealed that only two parameters are eventually estimable. It also enabled us to compare the performance of known detection systems relative to the quantum limit in absolute terms, a question left open in the literature. The gap identified by us should motivate the search for detection systems, ideally on a single copy of the light field on the image plane, seeking to reduce or eliminate it.
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Appendix A. Expressing the density matrix in the HG basis

The density matrix is written in terms of the kets $|\psi_i\rangle$, which are expressed in the position space as in equation (3). We assume a normalised Gaussian PSF of the form

$$\psi_{\text{PSF}}(x) = \frac{1}{(2\pi\sigma)^{1/4}} e^{-\frac{x^2}{4\sigma^2}},$$

(A.1)

and so

$$|\psi_i\rangle = \int dx \psi_{\text{PSF}}(x - \chi_i)|x\rangle.$$

(A.2)

The kets $|\psi_i\rangle$ can be expressed in terms of the complete HG modes as

$$|\psi_i\rangle = \sum_{q=0}^{\infty} \langle \phi_q | \psi_i \rangle |\phi_q\rangle,$$

(A.3)

where $|\phi_q\rangle$ are the HG modes, which can be expressed in the position space as [11]

$$|\phi_q\rangle = \frac{1}{(2\pi\sigma)^{1/4}} \frac{1}{\sqrt{2\pi q!}} \int dx H_q\left(\frac{x}{\sqrt{2\sigma}}\right) e^{-\frac{x^2}{4\sigma^2}} |x\rangle,$$

(A.4)

where $H_q(x)$ are the Hermite polynomials. The coefficients of the expansion equation (A.3) are

$$\langle \phi_q | \psi_i \rangle = \frac{1}{\sqrt{2\pi\sigma^2} 2q!} \int dx dx' H_q\left(\frac{x}{\sqrt{2\sigma}}\right) e^{-\frac{x^2}{4\sigma^2}} e^{-\frac{(x'-\chi_i)^2}{4\sigma^2}} (x|x').$$

(A.5)

Setting $\frac{x}{\sqrt{2\sigma}} = \alpha_i$ we get

$$|\alpha_i\rangle \equiv |\psi_i\rangle = \sum_{q=0}^{\infty} \frac{\alpha_i^q}{\sqrt{q!}} e^{-\alpha_i^2/2} |\phi_q\rangle,$$

(A.6)

which has the same mathematical form as the coherent states with $|\{\phi_q\}\rangle$ forming the Fock basis [39].

The state in equation (3) can be also written in terms of the displacement operators $D(\alpha_i) = e^{\alpha_i a^\dagger - \alpha_i a}$, with $\alpha_i = \frac{x_i}{\sqrt{2\sigma}} \in \mathbb{R}$

$$\rho_\alpha = \sum_i \sqrt{w_i} D(\alpha_i) |0\rangle \langle 0| \sqrt{w_i} D^\dagger(\alpha_i),$$

(A.7)

where $D(\alpha)$ is the displacement operator.

The derivative of each coherent state with respect to its real amplitude $\alpha$ is given by

$$\frac{\partial |\alpha\rangle}{\partial \alpha} = \frac{\partial D(\alpha)}{\partial \alpha} |0\rangle = (a^\dagger - \alpha) |\alpha\rangle,$$

$$\frac{\partial |\alpha\rangle}{\partial \alpha} = \frac{\partial D^\dagger(\alpha)}{\partial \alpha} |0\rangle = (\alpha - a) |\alpha\rangle,$$

(A.8)

which yields the formula equation (22).

Appendix B. Analytic results for $N$ sources

The Tracy–Singh product [53, 54] defined for matrices $A$ and $B$ subdivided into blocks $A_{ij}$ and $B_{kl}$ is $A \odot B$ where the $(i, j)$th block of $A \odot B$ is $A_{ij} \odot B$ whose $(k, l)$th block is in turn $A_{ij} \otimes B_{kl}$. That is if $A, B$ are block matrices with

then the Tracy–Singh product is

\[
A \otimes B = \begin{pmatrix}
A_{11} \otimes B_{11} & A_{12} \otimes B_{12} \\
A_{21} \otimes B_{11} & A_{22} \otimes B_{12}
\end{pmatrix}
\]

Using the above definition, the matrix of equation (31) is found to be

\[
(\Upsilon^{-1} \otimes \rho_A + \rho_A \otimes \Upsilon^{-1}) = \begin{pmatrix}
D_w \otimes v_{\alpha\alpha} + v_{\alpha\alpha} \otimes D_w & D_w \otimes v_{\alpha\alpha} + v_{\alpha\alpha} \otimes D_w & 0 \\
D_w \otimes v_{\alpha\alpha} + v_{\alpha\alpha} \otimes D_w & D_w \otimes v_{\alpha\alpha} + v_{\alpha\alpha} \otimes D_w & 0 \\
0 & 0 & 0
\end{pmatrix},
\]

where the elements of \( \Upsilon^{-1} \) can be found using the formula of blockwise inversion:

\[
\Upsilon^{-1} = \begin{pmatrix}
v_{\alpha\alpha} & v_{\alpha\alpha} \\
v_{\alpha\alpha} & v_{\alpha\alpha}
\end{pmatrix}
\]

The inverse of the block matrix \( \Upsilon^{-1} \) exists, because it is the Gramian matrix of the linear independent vectors \( |\alpha_i\rangle \).

For the QFIM elements we need to evaluate the inverse of the top left \( 3N^2 \times 3N^2 \) part of the matrix of equation (B.1) which we denote \( \mathcal{A} \). In order to obtain the inverse of \( \mathcal{A} \), we need to further partition \( \mathcal{A} \) as

\[
\mathcal{A} = \begin{pmatrix}
\varepsilon & \varphi \\

\varphi & \vartheta
\end{pmatrix}
\]

with

\[
\varepsilon = [D_w \otimes v_{\alpha\alpha} + v_{\alpha\alpha} \otimes D_w] \vartheta = [D_w \otimes v_{\alpha\alpha} + v_{\alpha\alpha} \otimes D_w]
\]

The inverse of \( \vartheta \) is

\[
\vartheta^{-1} = \begin{pmatrix}
D_w^{-1} \otimes v_{\alpha\alpha}^{-1} & 0 \\
0 & v_{\alpha\alpha}^{-1} \otimes D_w^{-1}
\end{pmatrix}
\]

The elements of \( \mathcal{A}^{-1} \) will be given by the formulas

\[
(\mathcal{A}^{-1})_{11} = (\varepsilon - \vartheta \vartheta^{-1} \varphi)^{-1} = S^{-1}
\]

\[
(\mathcal{A}^{-1})_{12} = -S^{-1} \vartheta \vartheta^{-1}
\]

\[
(\mathcal{A}^{-1})_{12} = -\vartheta^{-1} \varphi S^{-1}
\]

\[
(\mathcal{A}^{-1})_{22} = \vartheta^{-1} + \vartheta^{-1} \varphi S^{-1} \vartheta^{-1}.
\]

After calculations and by substituting the \( \Upsilon^{-1} \) elements from equation (B.3), we derive the explicit form of \( \mathcal{A}^{-1} \) elements:

\[
(\mathcal{A}^{-1})_{11} = S^{-1} = (\Upsilon^{-1}_{\alpha\alpha} \otimes D_w + D_w \otimes \Upsilon^{-1}_{\alpha\alpha})^{-1}
\]

\[
(\mathcal{A}^{-1})_{12} = S^{-1}(1 \otimes (\Upsilon^{-1}_{\alpha\alpha} \otimes v_{\alpha\alpha} \otimes \Upsilon^{-1}_{\alpha\alpha}) \otimes \mathbb{I})
\]

\[
(\mathcal{A}^{-1})_{21} = \left( \frac{1}{(\Upsilon^{-1}_{\alpha\alpha} \otimes v_{\alpha\alpha} \otimes \Upsilon^{-1}_{\alpha\alpha}) \otimes \mathbb{I}} \right) S^{-1}
\]

\[
(\mathcal{A}^{-1})_{22} = \left( \frac{D_w^{-1} \otimes v_{\alpha\alpha}^{-1} \otimes D_w^{-1}}{v_{\alpha\alpha}^{-1} \otimes D_w^{-1}} \right) + \left( \frac{1}{(\Upsilon^{-1}_{\alpha\alpha} \otimes v_{\alpha\alpha} \otimes \Upsilon^{-1}_{\alpha\alpha}) \otimes \mathbb{I}} \right) S^{-1}(\mathbb{I} \otimes (\Upsilon^{-1}_{\alpha\alpha} \otimes v_{\alpha\alpha} \otimes \Upsilon^{-1}_{\alpha\alpha}) \otimes \mathbb{I}).
\]
The QFIM elements are then obtained from equations (36) and (B.8)

\[
\mathcal{Q}_{ij} = 2w_iw_j[-2\alpha_i(E_i) (E_j) \begin{pmatrix} -2\alpha_j |E_j\rangle \\ |E_j\rangle \end{pmatrix} + \begin{pmatrix} -2\alpha_j \mathbb{I} \otimes \mathbb{I} \\ \mathbb{I} \otimes \mathbb{I} \end{pmatrix} \mathcal{A}^{-1}\begin{pmatrix} -2\alpha_j \mathbb{I} \otimes \mathbb{I} \\ \mathbb{I} \otimes \mathbb{I} \end{pmatrix} |E_j\rangle]
\]

\[
= 2w_iw_j(\mathbb{I} \otimes \mathbb{I} |E_i\rangle |E_j\rangle) + 2w_iw_j(\mathbb{I} \otimes \mathbb{I} |E_i\rangle) S^{-1}[\mathbb{I} \otimes \mathbb{I} |E_j\rangle]
\]

Finally, to complement the discussion in the main text, we present some further examples of the QFIM eigenvalues for \( N = 4, 5 \) sources and in figure B2 we present the eigenvalues of the QFIM for 3 sources in the case of unequal weights (relative intensities). Figure B2.

Figure B1. The eigenvalues of the QFIM for 4 (left) and 5 (right) sources with equal intensities. The sources are separating from each other by equal distances: \((\alpha_1, \alpha_2, \alpha_3, \alpha_4) = (x, 2x, 3x, 4x)\) and \((\alpha_1, \alpha_2, \alpha_3, \alpha_4, \alpha_5) = (x, 2x, 3x, 4x, 5x)\).

Figure B2. The eigenvalues of the QFIM matrix in the case of 3 sources. The sources are separating from each other at equal distances, i.e. \((\alpha_1, \alpha_2, \alpha_3) = (x, 2x, 3x)\). It can be noticed that the limiting values of the two non zero eigenvalues are different as the weights become different. However, the rank 2 of the QFIM remains. In figure (b) the limiting case of one extremely bright source and two very weak ones is displayed. The inset shows the two vanishing eigenvalues.
Appendix C. Analytic results for $x_i \ll \sigma$

The state in the sub-diffraction regime is given by equation (40). The derivative can be calculated immediately from this formula and it is

$$\frac{\partial}{\partial \alpha_i} p = -2\alpha_i |0\rangle \langle 0| + |0\rangle \langle 1| + |1\rangle \langle 0| + 2\alpha_i |1\rangle \langle 1| = \left( -2\alpha_i \frac{1}{1} \right)$$ \hspace{1cm} (C.1)

By solving the SLD equation $\partial_{\alpha_i} \rho_{\alpha} = (\rho_{\alpha} L_i + L_i \rho_{\alpha})$, we can determine the SLDs in the $\{0\rangle, |1\rangle$ basis:

$$L_i = \frac{2}{(C_2 - 1)C_2 + C_1^2} \begin{pmatrix} C_2 C_4 + (C_2 - C_1^2) \alpha_i & (C_2 - 1) C_2 + (C_4 - 2C_2 C_4) \alpha_i \\ (C_2 - 1) C_2 + (C_4 - 2C_2 C_4) \alpha_i & C_1 - C_4 C_2 + (2C_2^2 + C_4 - 1) \alpha_i \end{pmatrix}$$ \hspace{1cm} (C.2)

Knowing the SLDs, we can obtain the QFIM of equation (42).

As already mentioned in the main text, the rank of the QFIM only depends on the matrix

$$\begin{pmatrix} M_{11} & M_{12} \\ M_{21} & M_{22} \end{pmatrix}$$ \hspace{1cm} (C.3)

of equation (42), with the elements of this matrix given by equation (43). The eigenvalues $\mu_1, \mu_2$ of the matrix equation (C.3) are

$$\mu_1 = \frac{1}{2}(C_2^2 - \sqrt{(C_2 - 1)C_2 + 4C_1^2 - 1})^2 + 4(C_2 - 1)C_2 + C_1^2 \text{ and } C_2 = \frac{1}{2}(1 - \sqrt{1 - 4C_1^2})$$
$$\mu_2 = \frac{1}{2}(C_2^2 + \sqrt{(C_2 - 1)C_2 + 4C_1^2 - 1})^2 + 4(C_2 - 1)C_2 + C_1^2 \text{ and } C_2 = \frac{1}{2}(1 + \sqrt{1 - 4C_1^2})$$ \hspace{1cm} (C.4)

The condition for the eigenvalues to be zero is

$$\left(0 = 3C_2^2 - 1 - \sqrt{(3C_2^2 - 1)^2} \land \ C_2 = \frac{1}{2}(1 - \sqrt{1 - 4C_1^2}) \right) \lor \left(0 = 3C_2^2 - 1 \land \ C_2 = \frac{1}{2}(1 + \sqrt{1 - 4C_1^2}) \right).$$ \hspace{1cm} (C.5)

The first part $0 = 3C_2^2 - 1 - \sqrt{(3C_2^2 - 1)^2}$ is always true, as it reduces to the identity $(3C_2^2 - 1)^2 = (3C_2^2 - 1)$. For the second part we have

$$C_2 = \frac{1}{2}(1 \pm \sqrt{1 - 4C_1^2}) \iff (2C_2 - 1)^2 = 1 - 4C_1^2 \iff C_2^2 = C_2 + C_1^2 = 0.$$ \hspace{1cm} (C.6)

Substituting $C_2$ and $C_1$ we get

$$\left(\sum_{i=1}^{N} \alpha_i^2 \right)^2 - \sum_{i=1}^{N} \alpha_i^2 + \left(\sum_{i=1}^{N} \alpha_i^2 \right)^2 = 0 \iff \left(\sum_{i=1}^{N} \alpha_i^2 \right)^2 - \sum_{i=1}^{N} \alpha_i^2 + \sum_{i=1}^{N} \alpha_i^2 + 2 \sum_{i=1,j=1}^{N} \alpha_i \alpha_j = 0$$
$$\left(\sum_{i=1}^{N} \alpha_i^2 \right)^2 + 2 \sum_{i=1,j=1}^{N} \alpha_i \alpha_j = 0.$$ \hspace{1cm} (C.7)

Since $\alpha_i$ are strictly positive, except one that can be zero, this sum of positive terms cannot be equal to zero. Therefore, this statement is always false. Thus, the equation (C.5) becomes $(1 \land 0) \lor (1 \land 0) = 0$, which means that the two eigenvalues can never be zero and the QFIM will be rank 2.

Appendix D. Calculation of the QFI for the Sinc PSF

The expansion of the Sinc function on the HG modes is not ideal for numerical calculations. Instead we use the spherical Bessel function of the 1st kind and express the states onto those modes in which we then truncate. If the PSF is a sinc function, the $|\psi_i\rangle$ are

$$|\psi_i\rangle = \frac{1}{\sqrt{\sigma}} \int_{-\infty}^{\infty} \sin\left(\frac{\pi(x - X_i)}{\sigma}\right) dx.$$ \hspace{1cm} (D.1)

We can use the identity \[55]\]

$$\sin\left(\frac{\pi(x - x')}{\sigma}\right) = \sum_{q=0}^{\infty} (2q + 1) j_q\left(\frac{\pi x}{\sigma}\right) j_q\left(\frac{\pi x'}{\sigma}\right),$$ \hspace{1cm} (D.2)
where \( J_q(x) \) is the spherical Bessel function of the 1st kind. The spherical Bessel function are orthogonal in all \( \mathbb{R} \):

\[
\int_{-\infty}^{\infty} dx \, J_q(x) J_p(x) = \frac{\pi}{2q + 1} \delta_{qp},
\]

therefore we can define the orthonormal basis

\[
\left| j_q \right| = \sqrt{\frac{2q + 1}{\sigma}} \int_{-\infty}^{\infty} dx \, J_q \left( \frac{\pi x}{\sigma} \right) \left| x \right|.
\]

The set of the spherical Bessel functions is a basis in \( \mathbb{R} \), but is not complete since it is not a resolution of identity as we can see from equation (D.2). Hence, we can expand the sinc function on the bessel function basis, using the identity equation (D.2):

\[
\left| \psi \right| = \frac{1}{\sqrt{\sigma}} \int_{-\infty}^{\infty} \sum_{q=0}^{\infty} (2q + 1) J_q \left( \frac{\pi x}{\sigma} \right) J_q \left( \frac{\pi X_i}{\sigma} \right) \left| x \right| = \sum_{q=0}^{\infty} \sqrt{2q + 1} J_q \left( \frac{\pi X_i}{\sigma} \right) \left| j_q \right|.
\]

Using the identity for the Bessel functions

\[
\frac{\partial J_q(x)}{\partial x} = J_{q-1}(x) - \frac{q + 1}{2} J_q(x)
\]

we can also have an expression for the derivative of \( \left| \psi \right| \)

\[
\frac{\partial \left| \psi \right|}{\partial X_i} = \frac{\pi}{\sigma} \left( J_{q-1} \left( \frac{\pi X_i}{\sigma} \right) - \frac{q + 1}{2} J_q \left( \frac{\pi X_i}{\sigma} \right) \right)
\]

We see that both the state \( \rho \) and its derivatives are completely expressed within the basis \( \left| j_q \right| \). This means that we can use the definition of the SLD (equation (D.8)) and express the SLD in the same basis.

\[
2 \frac{\partial \rho}{\partial \delta_\mu} = \rho L^\mu + L^\mu \rho.
\]

In this way the fact that the specific basis is not complete does not affect our calculations.

For the numerical calculations we have to truncate our state in the appropriate amount of modes. From figures 6 and D1, we can see that our conclusions do not change with the use of a non-Gaussian PSF.

**Appendix E. Eigenvalues of the CFIM for SPADE and direct imaging**

Finally, we present the eigenvalues of the CFIM for SPADE and direct imaging for a large range of separations.
Figure E1. The eigenvalues of the CFIMs in the case of 9 sources for SPADE (left) and direct imaging (right). The sources are positioned at $\alpha_i = (i - 5)\lambda$.

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